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SECURITY CLASSIFICAT OF THIS PAGE (When Date Entered READ INSTRUCTIONS REPORT DOCUMENTATION PAGE REPORT NUMBER 2. GOVT ACCESSION NO. CIPIENT'S CATALOG NUMBER TPE OF REPORT & PERIOD COVERED 4. TITLE (and Subtitle) Analysis of Electrophysiological Signals from Animals Subjected to Biodynamic Stress Progress May 1977-July 1979 6. PERFORMING ORG. REPORT NUMBER 7. AUTHOR(s) CONTRACT OR GRANT NUMBER(s) Bernard Saltzberg N000-76-C-0911 NW Williams D. Burton, Jr. PERFORMING ORGANIZATION NAME AND AUDRESS PROGRAM ELEMENT, PROJECT, TASK Texas Research Institute of Mental Sciences Information Analysis Section Houston, Texas 77030 NR-207-011 11. CONTROLLING OFFICE NAME AND ADDRESS 12. REPORT DATE Office of Naval Research, Biological Sciences Div. 16-Augus t-1979 13. NUMBER OF PAGES Biophysics Program Code 444 Arlington, Virginia 22217
14. MONITORING AGENCY NAME & ADDRESS(IT different from Controlling Office) 15. SECURITY CLASS. (of this report) Unclassified 154. DECLASSIFICATION/COWNGRADING 16. DISTRIBUTION STATEMENT (of this Report) Distribution of this report is unlimited. 17. DISTRIBUTION STATEMENT (of the abetract entered in Block 20, Il different from Report) AUG 27 1979

18. SUPPLEMENTARY NOTES

19. KEY WORDS (Continue on reverse side if necessary and identify by block number)

Biodynamic stress, electrophysiological signals, EEG, evoked potentials

The objective of the signal analysis and data processing reported here was to detect and evaluate the effects of impact acceleration on the functional integrity of the nervous system as revealed by electrophysiological recordings. Evoked potential methods were used to evaluate the effects of impact acceleration on afferent nerve impulse transmission. The methods of period analysis, concordance, and power spectra were used to study the effect of impact acceleration on background EEG activity. Consistent impact dose related effects were-

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20. Abstract (continued)

observed on the time course of recovery of the amplitude and latency of evoked response components measured from single and small sample average evoked potentials. The analysis of background EEG activity showed clear changes between pre- and post-acceleration, but the magnitude of these changes did not show a consistent relationship to the level of acceleration.

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OFFICE OF NAVAL RESEARCH
Contract NO0014-76-C-0911
Task No. NR-207-011

PROGRESS REPOT, NO. 1. May 77-Jul 79,

Analysis of Electrophysiological Signals
from Animals Subjected to
Biodynamic Stress

Bernard/Saltzberg
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Analysis of Electrophysiological Signals from Animals Subjected to Biodynamic Stress

PROGRESS REPORT

Introduction:

The objective of the signal analysis and data processing performed on this project, and summarized in this report, was to detect and evaluate effects of impact acceleration on the functional integrity of the nervous system as revealed by electrophysiological (EEG) recordings. The analysis was performed on EEG data recorded at the Naval Aerospace Medical Research Laboratory (NAMRL) during biodynamic experiments using Rheusus monkeys. Using this data base a comprehensive series of analyses has been conducted at this institute (TRIMS) to study EEG evoked potential and background EEG activity before, during, and after the animals were subjected to various levels of impact acceleration. The data studied at TRIMS covers experiments conducted at NAMRL during the period January, 1975 through October, 1978, which involved acceleration runs in the -GX direction.

The methods of period analysis, concordance, and power spectrum were used to study the effect of acceleration on background EEG activity. Each of these methods showed changes between pre- and post-acceleration. However the changes did not follow a clear impact level (dose-response) relationship.

Evoked potentials were used to study the effect of impact acceleration on ascending nerve impulse transmission. Computer software was developed for analysis of single and small sample average evoked potentials. A series of analysis experiments was carried out which showed consistent dose related effects on the time course of recovery of amplitude and latency

of components of the evoked potential. This finding suggests that these measures may provide a reliable quantitative basis for assessing effects of biodynamic stress on nerve transmission.

Period Analysis - Methods:

Period Analysis - Results:

Four EEG data channels were digitized from analog tape to 10-bit precision at 2 millisecond sample intervals using an AR-11 analog digital converter on PDP-11 computer. The digitized data was analyzed using period analysis (Saltzberg et al, 1966). In this method the number of both positive and negative going baseline crossings of the data in each 10-second epoch was counted.

The resulting 10 second counts were smoothed using a 1-minute (6-epoch) running average. The smoothed counts were plotted for each channel. Figures A1 through A11 are the plots for the experimental runs listed in Table 1. The time of the acceleration event is indicated on the plots by an arrow at time 0.0. In order, from top to bottom in these plots the channels are: Right Motor-Sensory, Right Sensory-Sensory, Left Sensory-Sensory, and Left Motor-Sensory.

Table 1 also indicates 1) the average reduction in the baseline crossing rate, relative to the pre-event rate, averaged over 4 channels, and 2) the time to recovery of variability in the rate, measured from the plots.

In the non-fatal runs, the effect of acceleration is shown as a decrease in the baseline crossing rate. The effect is not clearly dependent on the level of acceleration. In general, the minute-to-minute variability of the baseline cross rate is also reduced immediately following acceleration. The time to recovery of variability as measured from the plots is likewise not strongly dose dependent.

Table 1
PERIOD ANALYSIS SUMMARY

Animal	Run	Acceleration G	Reduction in Baseline Cross Rate (1)	Time To Recovery of Variability (2)
A0-3921	LX-1364	40	0.39	2.0 min
(Rob't Rhes.)	LX-654	50	0.63	7.3 min
A0-3948	LX-1891	80	0.26	7.0 min
A0-3948	LX-1892	81	0.40	13.1 min
A0-3935	LX-1362	105	0.82	10.0 min
A0-3933	LX-1894	106	0.20	39.0 min
A0-3924	LX-1893	108	no change	no change
A0-4099	LX-1359	109.7	0.12	3.6 min
A0-3921	LX-1365	110	-(3)-	-(3)-
A0-3935	LX-1363	127	0.33	2.0 min
A0-4099	LX-1360	130	-(3)-	-(3)-

Notes:

- (1) Average of reduction in crossing rate (pre-post)/pre for four channels
- (2) Average of recovery time for four channels
- (3) Fatal run

Concordance - Methods:

Saltzberg (1975) proposed that a running computation of the Kendall-W Coefficient of Concordance would provide a dynamic indication of the time course of similarity among multiple EEG channels. Based on this idea, a program has been written which implements the computation of the Kendall-W including correction for the presence of ties in the input data. In computing the coefficient of concordance, the input data for each epoch in the window is ranked (within channels). The sum of the ranks across channels for each epoch is computed. It is the variance of the resulting sum of ranks, compared to the maximum variance (which would occur if there were complete agreement) which determines the Kendall-W.

Four channels of EEG data were digitized and the baseline crossing. .

rate was determined for each 10 second epoch of each channel (see Period

Analysis - Methods). Each EEG channel (excluding the stimulus mark) is

considered an independent measurer of the EEG over a window of 3 minutes

(18, 10-second epochs). The concordance computation is arranged to report

how well the EEG channels agree in their ranking of activity (baseline

crossings) over the window (Figure 1).

To track the concordance over a period of time, the Kendall-W is recomputed every 10 seconds by deleting data from the oldest epoch in the 3 minute window and inserting data from the next epoch to enter the window. Concordance - Results:

The results of computing concordance on the data listed in Table 2 are shown in the plots. Figures B1 through B11. The following general results were noted. First, that the level of concordance varies

FIGURE 1 ILLUSTRATION OF CONCORDANCE COMPUTATION

Step A. Raw Data-Baseline Crossings

		,	Epoch								
Chann	e1	1_1_	2	3	4	5	6				
	1	20	25	23	26	28	30				
	2	18	19	20	21	22	23				
	3	17	16	15	18	19	20				
	4	22	26	23	28	30	29				

Step B. Ranking of Data within channels, across epochs

• • • • •	••••	-		- t+	ech (J)	••	······································
Chai	nnel	1	2	3	4	5	6	
	1	1	3	2	4	5	6	
	2	1	2	3	4	5	6	
	3	3	2	1	4	5	6	
	4	1	3	2	4	6	5	
Sum (Ranks	of (R _j)	6	10	8	16	21	23	$14 = \overline{R} = Mean (R_j)$

Step C. Computation

k = number of channels (4)

N = number of epochs (6)

s = sum of squared deviations
$$s = \sum_{j=1}^{N} (\overline{R} - R_j)^2 = 250$$

Maximum possible sum of squared deviations = M

$$M = \frac{1}{12} k^2 (N^3 - N) = 280$$

Kendall W =
$$\frac{s}{M}$$
 = $\frac{250}{280}$ = 0.89

Table 2
CONCORDANCE SUMMARY

<u>Animal</u>	Run	Acceleration (G)	Maxium Concordance Reduction (1)	Time To Recovery (Minutes) (2)
A0-3921	LX-1364	40	no effect	no effect
(Rob't Rhes.)	LX-654	50	.70	7.4
A0-3948	LX-1891	80	.38	7.5
A0-3948	LX-1892	81	.58	14.9
AQ-3935	LX-1362	105	.47	6.7
A0-3933	LX-1894	106	.53	10.5
A0-3924	LX-1893	108	.46	9.1
A0-4099	LX-1359	109.7	.58	10.9
A0-3921	LX-1365	110	-(3)-	-(3)-
A0-3935	LX-1363	127	.55	5.0
A0-4099	LX-1360	130	-(3)-	-(3)-

Notes:

- (1) Maximum Reduction in value of Kendall-W following impact relative to pre-impact average.
- (2) Time to first return to pre-impact level of Kendall-W
- (3) Fatal run

in most animals in a cyclic fashion. Second, that the onset of a stimulation period appears to affect the concordance in either of two directions depending on the concordance level prior to stimulus onset. For concordance values less than 0.5, the concordance is increased following the start of stimulation. The effect is to reduce the concordance if the initial concordance was greater than 0.5. The effect of acceleration is an immediate decrease in the level of concordance. The effect continues for a number of minutes but the time of recovery to the pre-acceleration concordance is not clearly dependent on the amount of acceleration. Table 2 summarizes the results obtained.

Power Spectrum - Methods:

Power Spectral Densities (PSDs) were computed on all four EEG channels for selected segments of tape LX-1894 106G (Subject A0-3933). For this analysis, 10 second epochs were taken 10 minutes, 5 minutes, and 30 seconds pre-impact and 1, 2, 5, 10, 20 and 30 minutes after impact. The analog data from each channel was sampled at 10 millisecond intervals (Nyquist Frequency = 50 Hz) using the Time/Data-100 computer. The computed power spectra were transferred to the PDP-11 where they were smoothed using a 0.5 Hz triangular weighted filer, and then plotted. The smoothed spectra are shown in Figures C1 through C36. Power is reported in arbitrary units.

Power Spectrum - Results:

All channels show an effect following impact. The PSD shows the bulk of its power at very low frequency immediately after impact compared to the pre-impact PSDs. This effect persists until 30 minutes post-impact,

by this time, the shape of the PSD is virtually identical to that found prior to impact. This most clearly seen in the Right Motor-Sensory lead. This result is consistent with the drop in the baseline crossing rate at the time of acceleration.

The Left Sensory-Sensory lead shows "ripples," separated by about 2 Hz. This begins with the PSD at 2 minutes post-impact and continues through the PSD at 20 minutes post impact. A ripple is also suggested in the data from the Left Motor-Sensory lead in the period from 2 minutes to 20 minutes post impact. Ripples in the power spectrum are indicative of the presence of recurrent transients imbedded in the complex EEG signal (Saltzberg, 1976). The ripple frequency of 2 Hz implies an underlying transient which is recurring at intervals of 0.5 seconds.

Evoked Potentials - Methods:

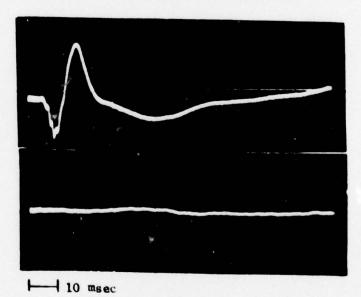
Evoked potentials (EPs) were obtained from monkeys stimulated in the spinal cord while simultaneously recording from the motor cortex (MX). The stimulus marker was used to trigger data acquisition at high sample rates from the MX channel of the analog tape. The data was digitized for 50 milliseconds following the stimulus using the PDP-11 computer, digitized EPs were written on digital tape for later averaging and peak measurements.

In an early trial, a sample interval of 0.125 milliseconds was used (8000 samples/second). It was found that the measured latency of peaks in the evoked potentials showed no variability prior to impact, indicating insufficient time resolution. The sample interval was reduced to 0.050 milliseconds (20,000 samples/second) which was found to preserve pre-impact variability in latency of evoked potential components.

Acceleration runs LX-3008 (20 GX), LX-3009 (80 GX), and LX-3010 (100 GX) on animal A-0761 have been studied in detail. It was possible in this

animal to detect single evoked potentials from the MX lead from spinal cord stimulation. Figure 2 shows typical averaged EP waveforms obtained from this animal. The top trace is the average of 25 responses prior to acceleration the bottom trace is the average of 25 responses beginning 1 second after the 100 GX acceleration. For the following discussion the negative-going component occurring at about 10 milliseconds is labeled N1, the positive component at 20 milliseconds is labeled P; and the longer negative wave is N2.

Figure 2
Typical Average Evoked Potential



Run LX-3010 Average of 25

Channel 1, Motor Corte Pre impact

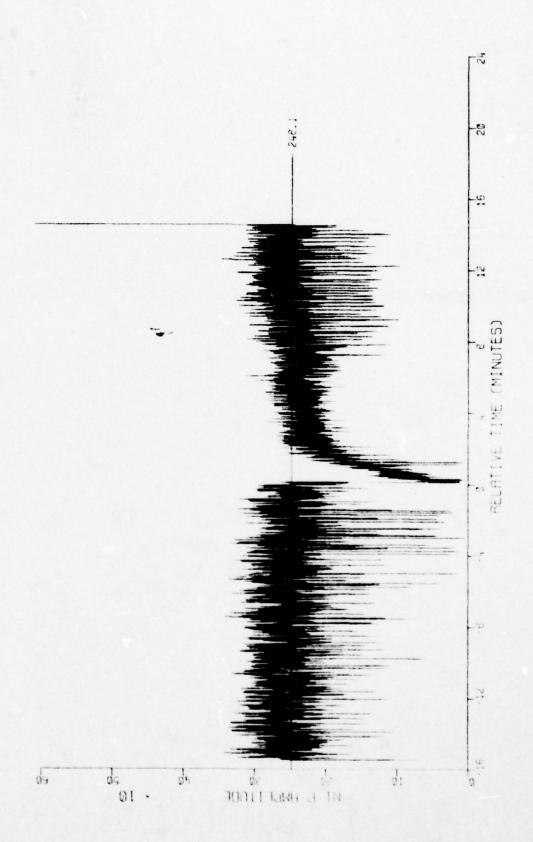
Channel 1, Motor Corte: Post 100 GX impact

In order to track changes in the amplitude and latency of the evoked potentials, a computer program was written which would read digital tapes of digitized EPs, average a selectable number of responses and measure amplitude and latency of the N1, P, and N2 components. After averaging

the zero level was set by subtracting the mean amplitude of the first 5 milliseconds from all points of the EP. Component amplitudes were referenced to this zero level. Amplitude is reported in arbitrary units since calibration information was not available on the analog tapes. Latency was measured from the fall of the stimulus pulse. The program also derived measures of peak-to-peak (N1-P, and P-N2) amplitude, latency, and slope. A total of 12 parameters is therefore measured for each evoked potential (3 latencies, 3 amplitudes, and 2 each peak-to-peak amplitudes, times, and slopes).

Figure 3 shows a plot of the N1-P amplitude for single responses from run LX-3010. There is a clearly defined effect of the impact acceleration (at time 0.0). However, because of the variability of the peak-to-peak amplitude from response to response, it is difficult to resolve the time course of recovery. To overcome this, and enable estimation of response variability, an analysis using average evoked potentials was made.

Five single EPs were averaged to create an Average EP (AEP). The twelve parameters were then measured from each average. Measures from ten successive averages were used to compute the mean and standard deviation for each measure. Each mean thus computed represented an estimate of the parameter over an epoch of about 10 seconds, (the actual epoch length was determined from the stimulus rate). The measures were plotted and are shown in Figures D1 through D36. Times shown in the plots and Table 3 are to the center of the epoch relative to the impact event. The mean of each measure in each epoch is the center line in the plots. The upper and lower plot lines indicate envelope of the mean plus and minus one standard deviation for that epoch. The grand mean and



ANIMAL A-0751 STIMULUS SITE 5. AFFER, RECORDING SITE 1. MX

ACCELERATION 100.0 G RATE 5.0 /SEC NBR. AVERHGED 1

FIGURE 3

standard deviation for measures from all pre-impact AEPs was also computed. The pre-impact grand mean is shown as the horizontal line on the plots.

Evoked Potentials - Results:

All parameters of the evoked potential show a clear effect on impact at accelerations above 20 G. The effects are an increase in the latency of N1 and P components and a decrease in amplitude of all components. The latency of the N2 components does not appear to be affected, however, this may be due to poor detection of the true position of that component. At the 20 G acceleration the amplitude of the P component was reduced slightly, but its latency and measures on the other components did not appear to be affected.

Table 3 is a summary of the effects of impact acceleration at various G levels on the measured parameters of the evoked potential. The table lists, for each parameter: 1) the pre-impact grand mean and standard deviation, 2) the mean and standard deviation for the first (10 second) epoch post-impact, and 3) the "recovery time" of the parameter. The recovery time for a parameter is defined as the time to the center of the first post-impact epoch whose mean is within an envelope of plus or minus one standard deviation of the pre-impact grand mean. If the epoch mean does not fall outside this envelope following impact then the recovery time is defined to be zero. The detailed measurement of the recovery time is made from computer printed listings of epoch statistics (mean, standard deviation).

Table 3
Evoked Potential Summary

		20G LX-3008		80G LX-3009		100G LX-3010	
Measure	mean	(s.d.)	mean	(s.d.)	mean	(s.d.)	
N1 Amplitude							
Pre-impact mean	-112.2	(6.5)	-111.1	(6.7)	-103.8	(6.9)	
First epoch post	-113.1	(6.0)	- 71.8	(44.4)	- 76.8	(41.7)	
Recovery time	0		127.8 s	ec	251.0 sec		
N1 Latency (msec)							
Pre-impact mean	9.44	(0.06)	9.24	(0.06)	9.02	(0.06)	
First epoch post	9.42	(0.06)	9.75	(0.57)	9.35	(2.35)	
Recovery time	0		158.6 s	ec	>866. se	ec	
P Amplitude							
Pre-impact mean	146.4	(28.7)	151.1	(29.1)	139.8	(27.8)	
First epoch post	95.4	(11.5)	66.9	(53.2)	83.8	(47.0)	
Recovery time	35.2 se	c	97.0 sec		107.3 sec		
P Latency (msec)							
Pre-impact mean	17.10	(0.37)	16.64	(0.36)	16.30	(0.25	
First epoch post	17.00	(0.31)	23.70	(7.10)	19.49	(8.61	
Recovery time	0		66.2 sec		497.2 sec		
N2 Amplitude							
Pre-impact mean	- 74.2	(11.4)	- 79.0	(11.7)	- 71.5	(12.8)	
First epoch post	- 60.7	(8.8)	- 32.0	(38.0)	- 54.0	(29.1)	
Recovery time	0		168.9 sec		189.0 sec		
N2 Latency							
Pre-impact mean	43.92	(3.32)	43.71	(2.58)	42.57	(2.4	
First epoch post	41.74	(3.04)	44.15	(2.35)	42.30	(4.60	
Recovery	0		0		0		
N1-P time (msec)							
Pre-impact mean	7.66	(0.37)	7.40	(0.36)	7.37	(0.26	
First epoch post	7.54	(0.30)	13.91	(6.77)	10.14	(6.76	
Recovery time	0		25.2	sec	0		

Table 3 (continued)

Evoked Potential Summary

Measure		20G LX-3008 mean (s.d.)		80G LX-3009 mean (s.d.)		100G LX-3010 mean (s.d.)	
N1-P	Amplitude Pre-impact mean First epoch post	258.6 208.5	(30.0) (10.3)	262.2 138.7	(31.2) (96.5)	243.7 160.7	(30.1) (8.8)
	Recovery time	35.2 sec		97.0 sec		138.1 sec	
N1-P	Slope Pre-impact mean First epoch post	33.7 27.6	(3.1)	35.4 16.3	(3.5) (14.0)	33.5 21.7	(3.8) (12.5)
	Recovery time	35.2 sec		138.1 sec		400.1 sec	
P-N2	Time (msec) Pre-impact mean First epoch post	26.82 24.78	(3.12) (2.99)	27.97 20.49	(2.40) (5.36)	26.27 22.81	(2.32) (7.70)
	Recovery time	0		25.2 s	ec	0	
P-N2	Amplitude Pre-impact mean First epoch post	220.7 156.1	(27.9) (10.9)	230.1 98.9	(30.2) (79.6)	221.4 137.9	(28.0) (7.3)
Recovery time		35.2 sec		168.9 s	ec	353.6 sec	
P-N2	Slope Pre-impact mean First epoch post	-8.26 -6.37	(0.85) (0.72)	-8.50 -4.21	(0.88) (2.91)	-8.06 -1.90	(0.93) (0.72)
Recovery time		45.4 se	С	179.2 s	ec	363.8 s	ec

Notes:

- (1) Amplitudes are in arbitrary units
- (2) Latencies are in milliseconds relative to stimulus
- (3) Slopes are computed as $\frac{\Delta}{\Delta}$ Amplitude

The recovery times of N1, and P amplitudes and latencies show a clear dose-response relationship with increasing acceleration. At 100 G acceleration the latency of the N1 component has not recovered by the end of the available data, 14 minutes 26 seconds post impact. The N2 component was not measurably affected, however this may be due to uncertainty in detection of the peak. Visible in Figure D 27 is a reduction in the variability (standard deviation) of the P amplitude for a period of approximately 10 minutes post impact at 100 G. This effect is not visible in the plot at 20 G, but does show up in the plot for 80 G where the variability takes about 4 minutes to recover to its pre-impact level.

Future Work:

We have demonstrated the ability to detect and quantify changes in small sample average evoked potentials from animals subjected to impact acceleration stress. This work should be expanded to include similar analysis of other acceleration runs with afferent stimulation to quantify EEG changes at intermediate acceleration levels. Data of this type is presently available on analog magnetic tape at TRIMS. Also, similar analysis using data, from monkeys receiving central (efferent) stimulation with spinal cord recording should be done.

In cases where single evoked potentials can be unambiguously detected, additional analysis should be directed to the problem of precisely determining the time course of changes taking place in nerve transmission during the period of acceleration. This aspect of future analytical research is of special value since it can lead to accurate measurement of the point on the acceleration profile when neural transmission is affected.

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 A Method for Determining Peaks in Average Evoked Potentials. (Submitted to Digital Equipment User's Society Fall Symposium, December 10-13, 1979).

Figures A1 - A11

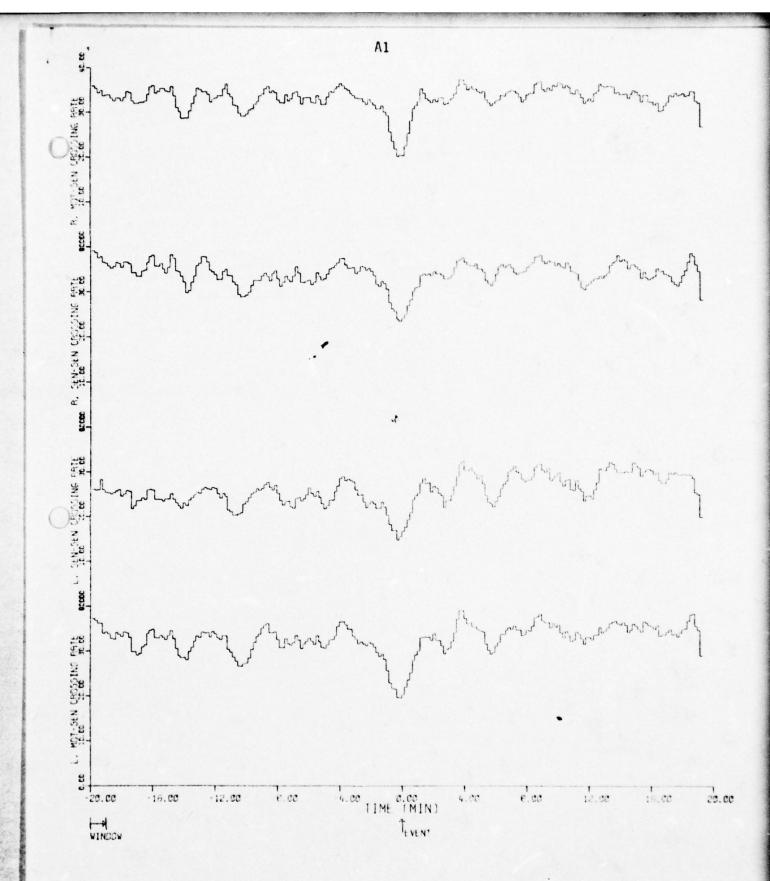
Period Analysis Summary Plots

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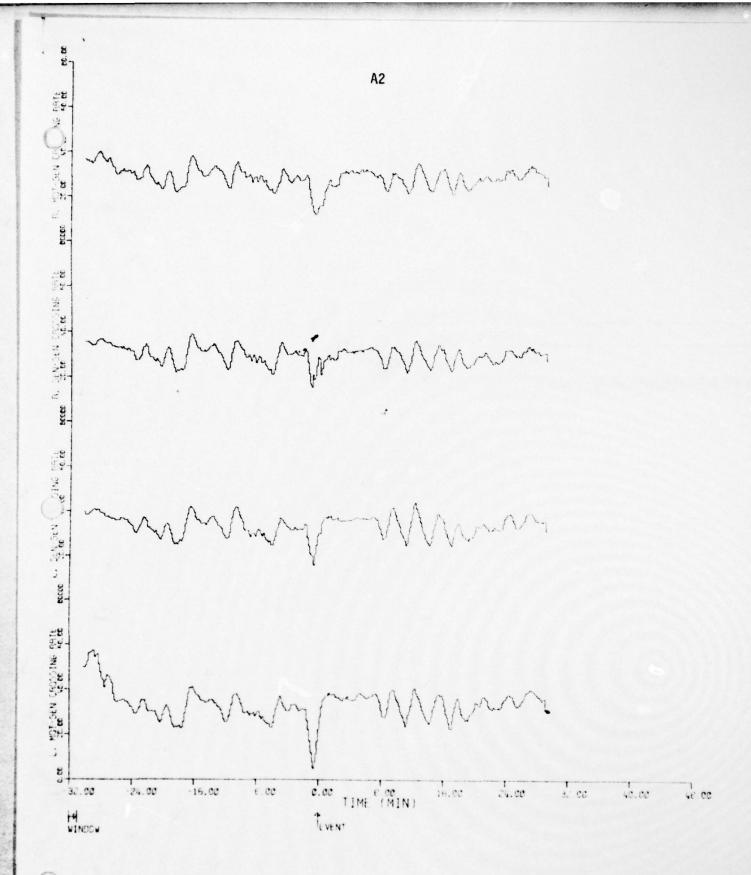
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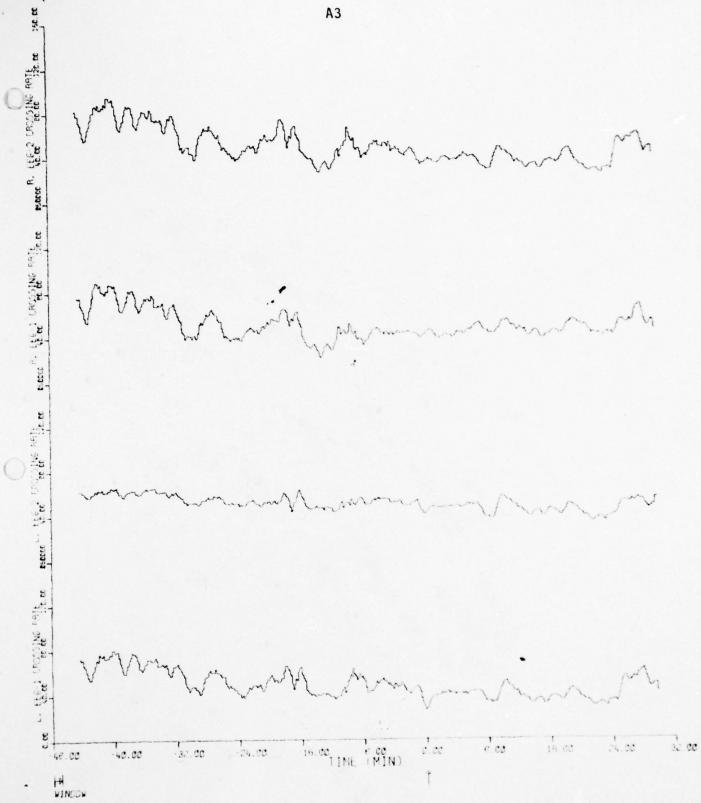
4 CHANNELS
10. SEC EPOCHS 6 AVERAGED
SNBJECT A0-3921 TAPE 1364 40GX



BASELINE CROSSINGS VERSUS TIME

4 CHANNELS
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SUBJECT ROBT RHESU TAPE 654 50GX

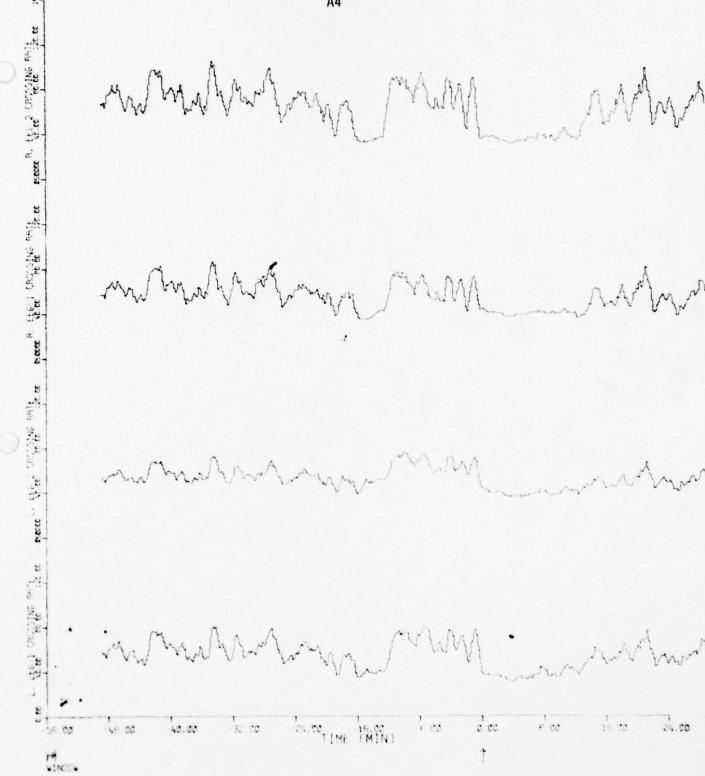




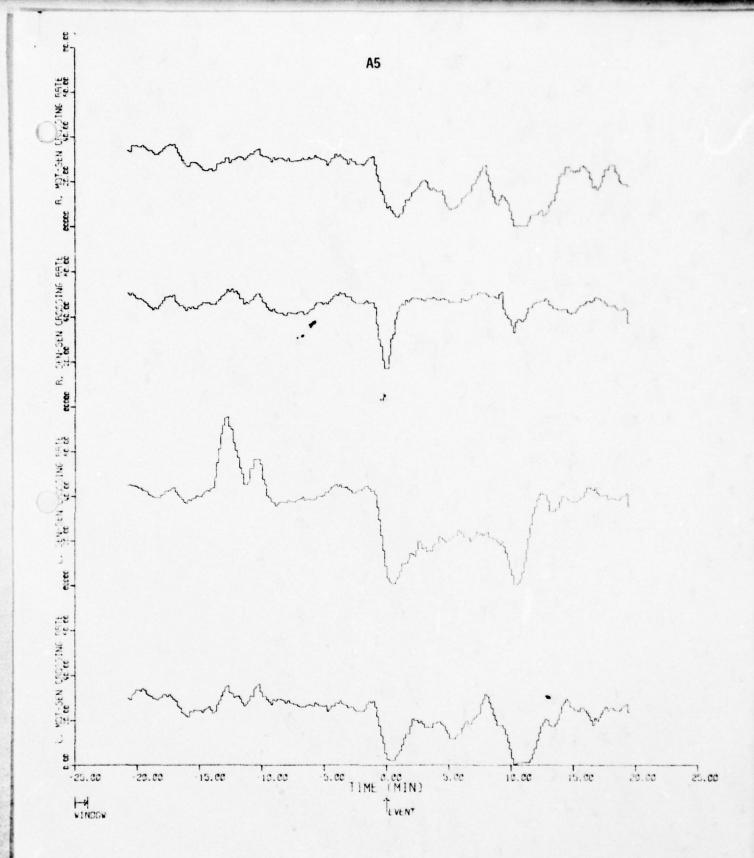
BASELINE CROSSINGS VERSUS TIME

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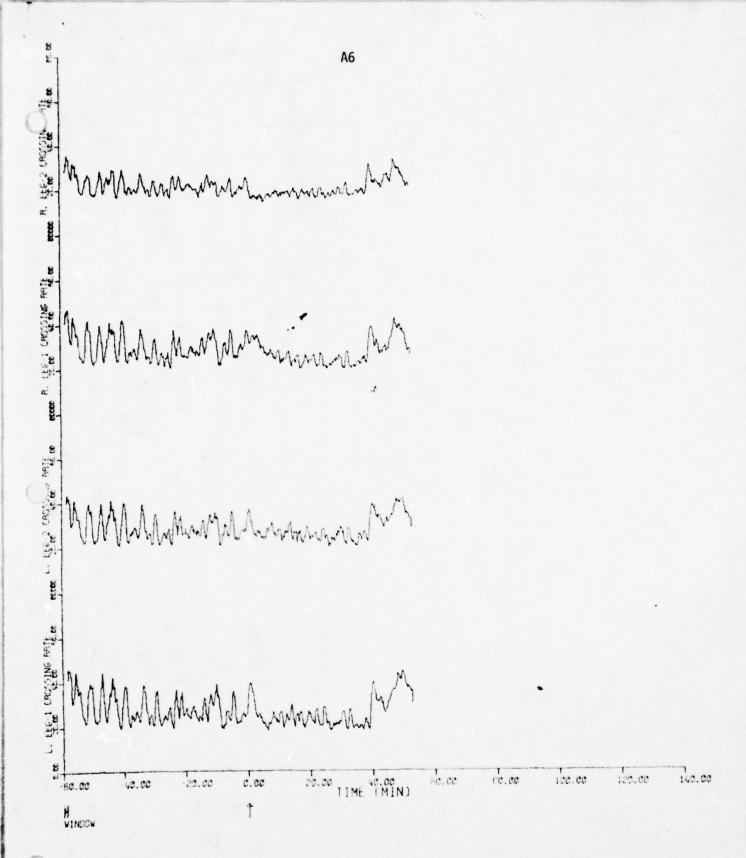




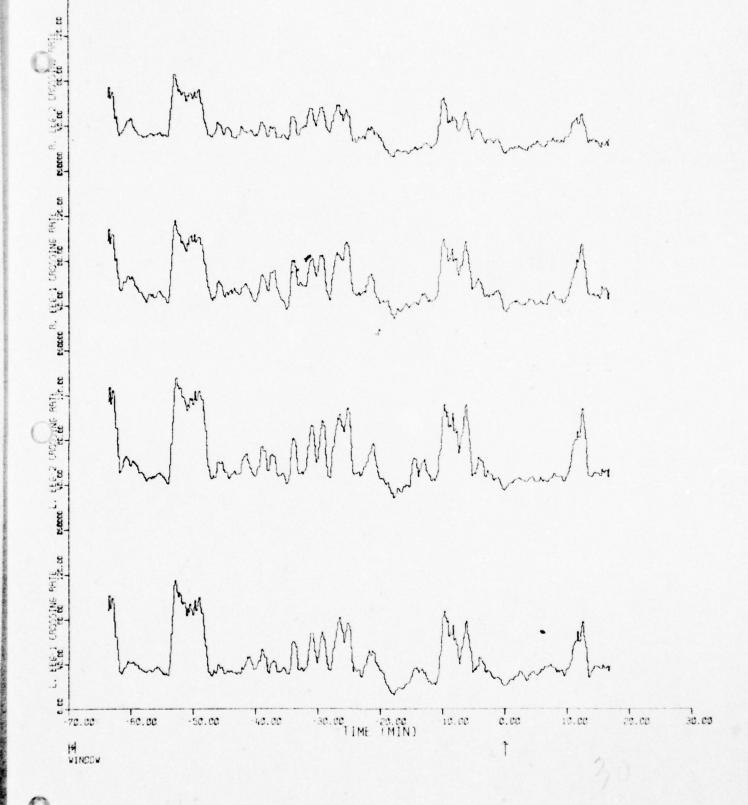
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4 CHANNELS 10. SEC EPOCHS 6 AVERAGED \$NBJECT 80 3935 TAPL 1362 105GX

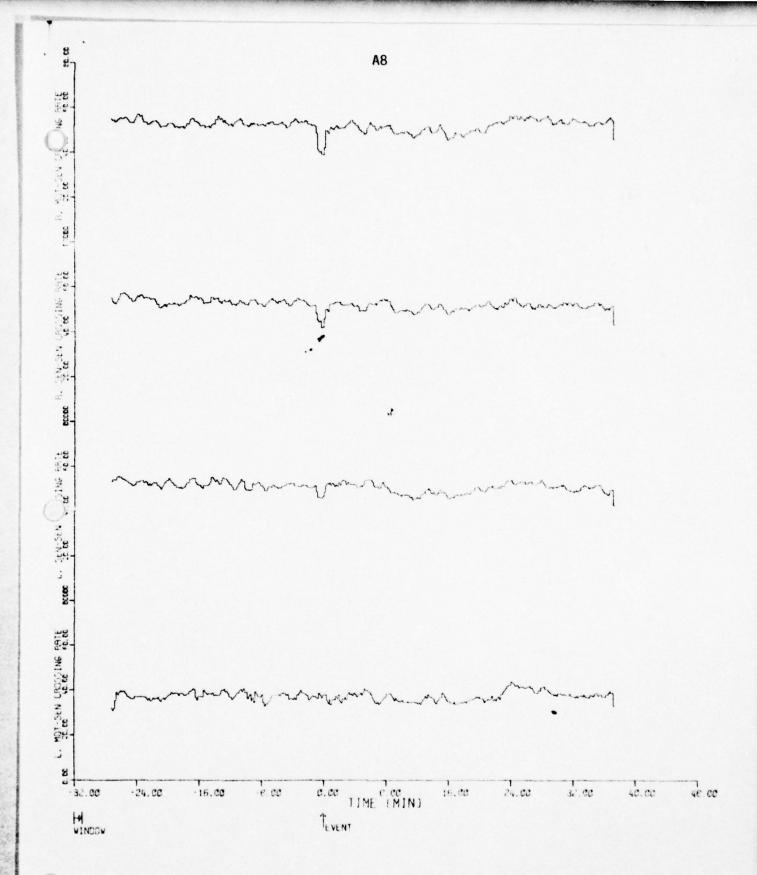


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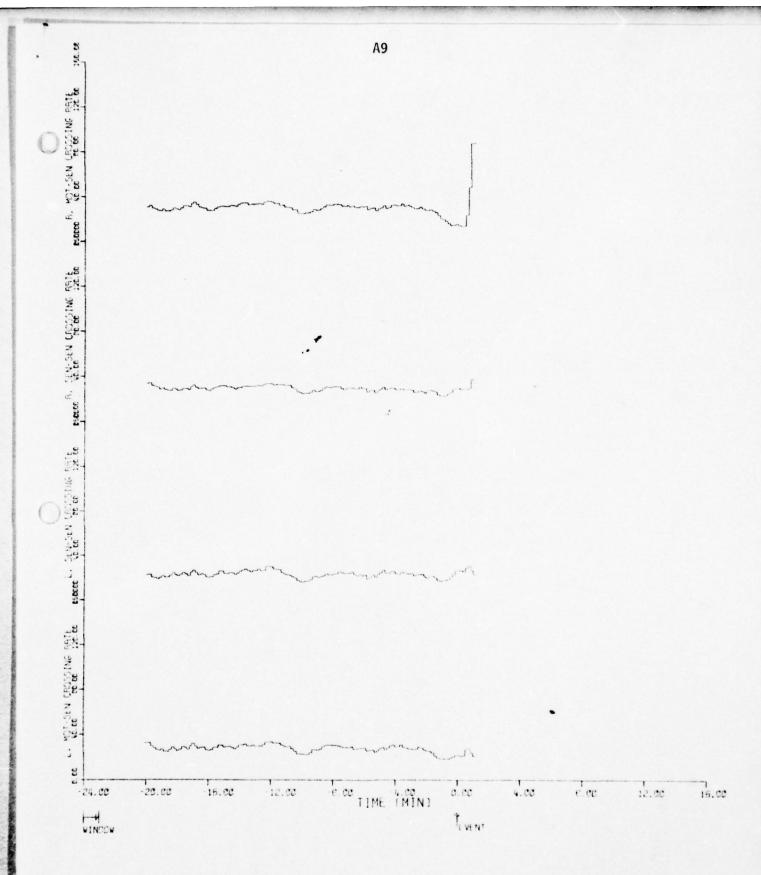


BASELINE CROSSINGS VERSUS TIME

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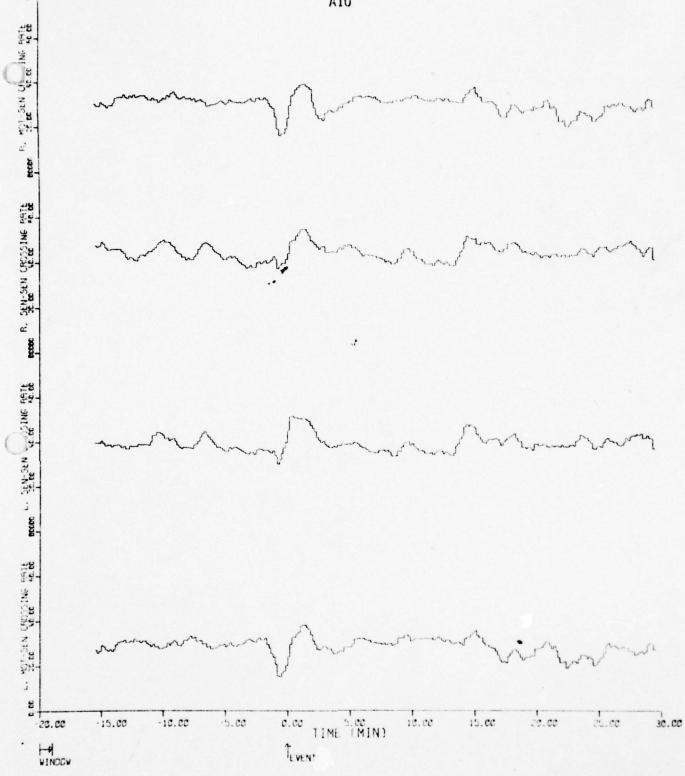
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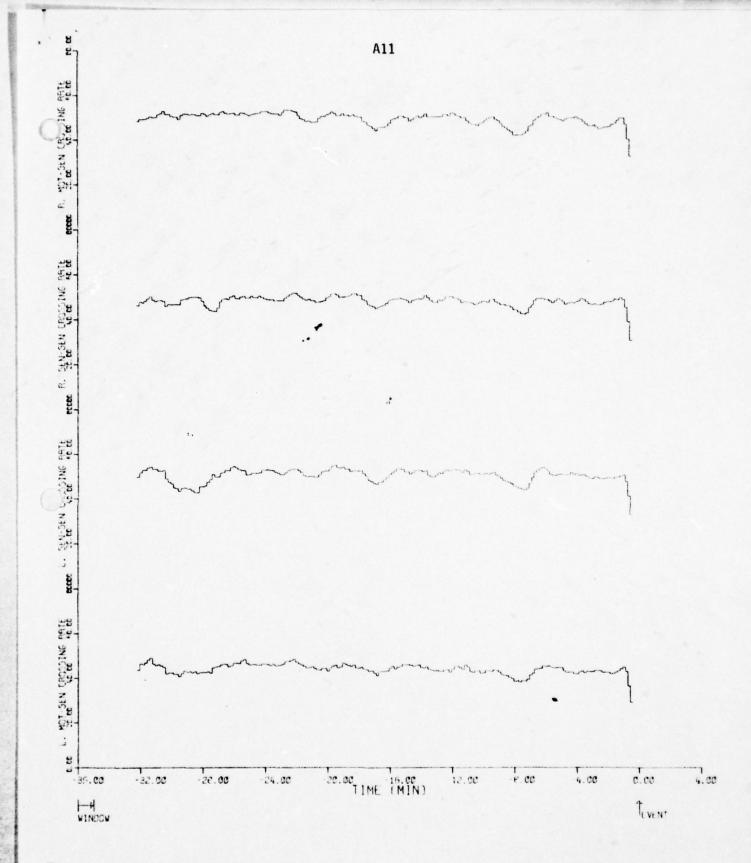
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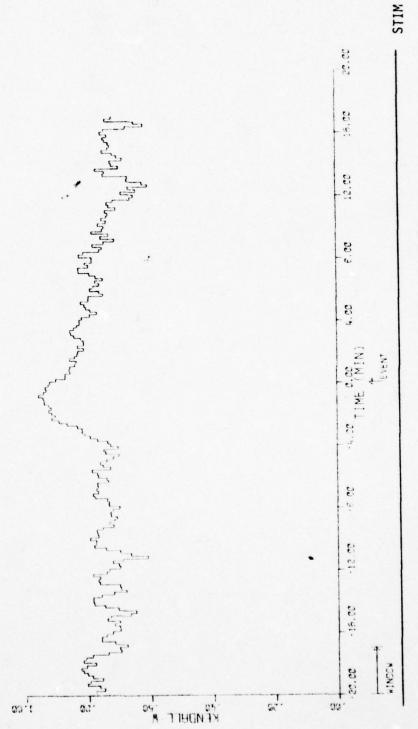


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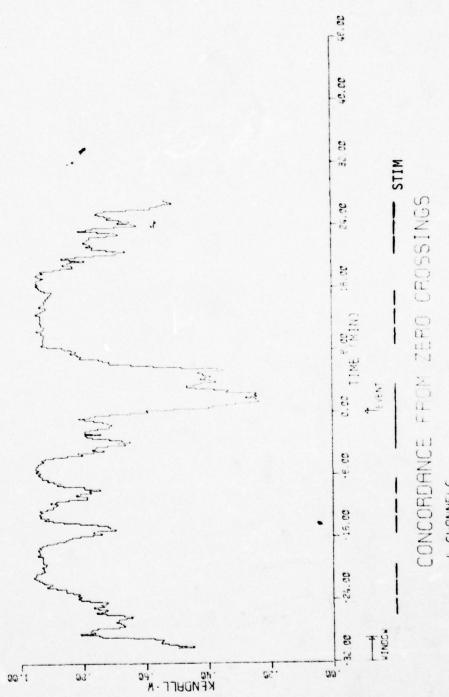
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Concordance Analysis Summary Plots

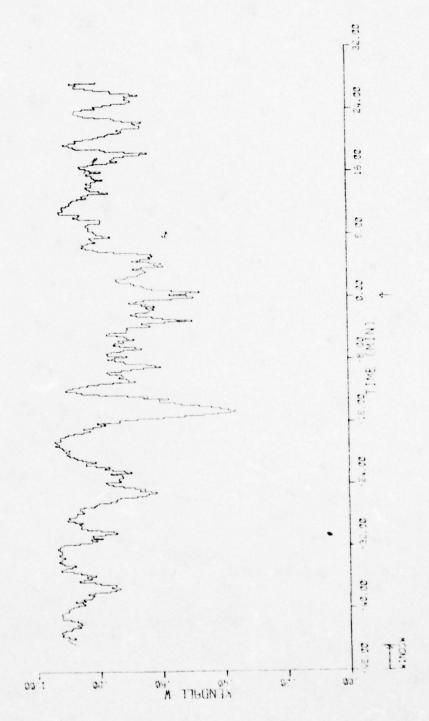


CONCORDANCE FROM ZERO CROSSINGS

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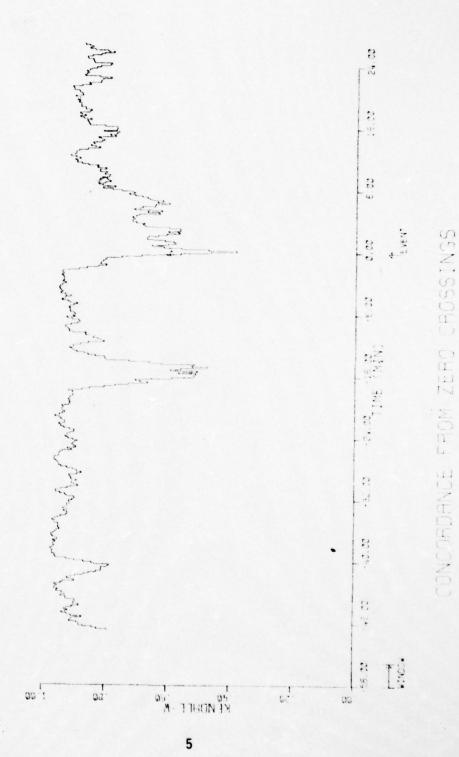


CONCORDANCE FROM ZERO CROSSINGS

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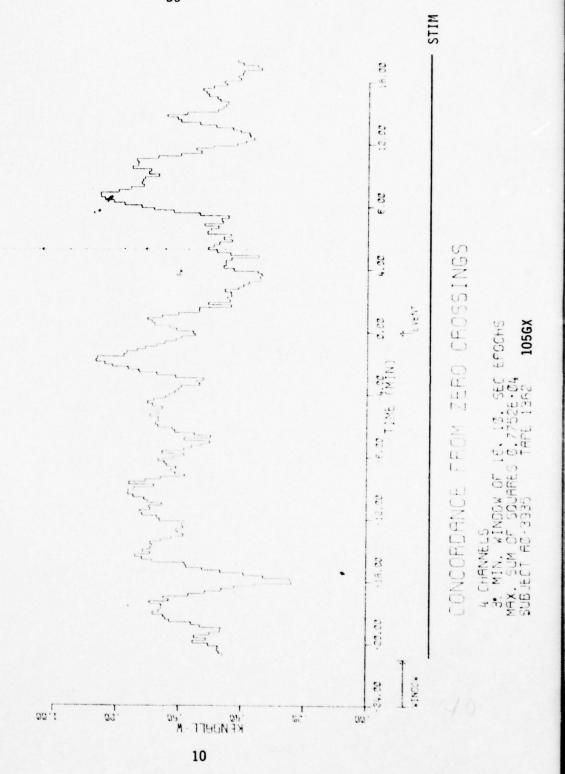
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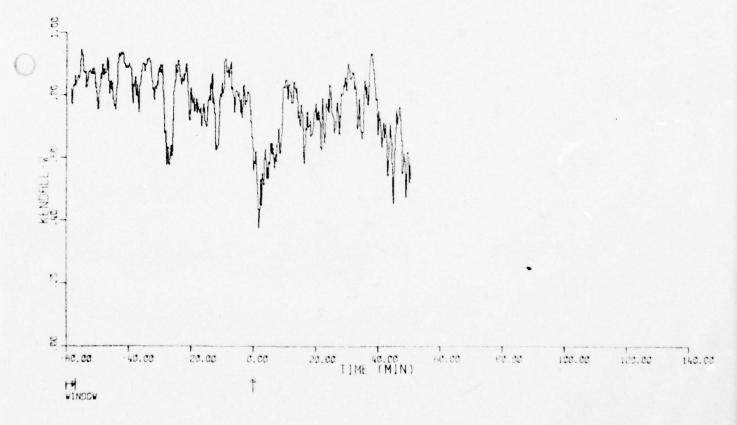
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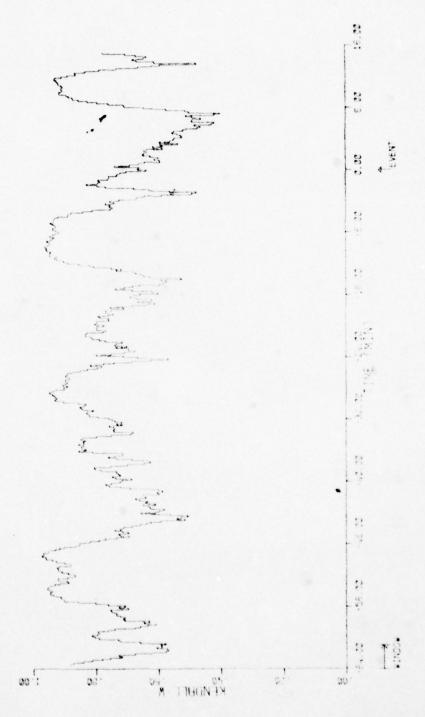
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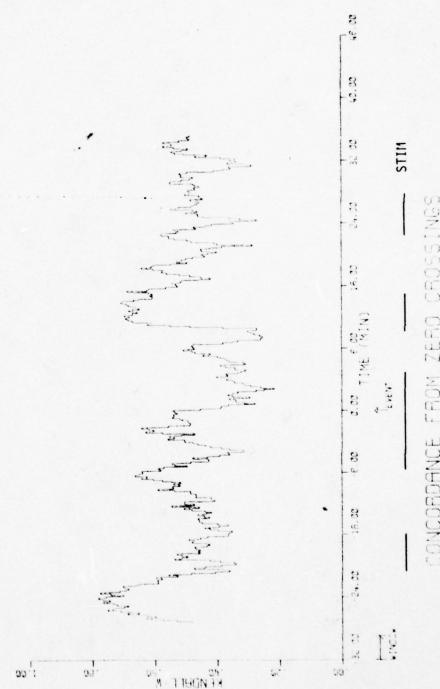
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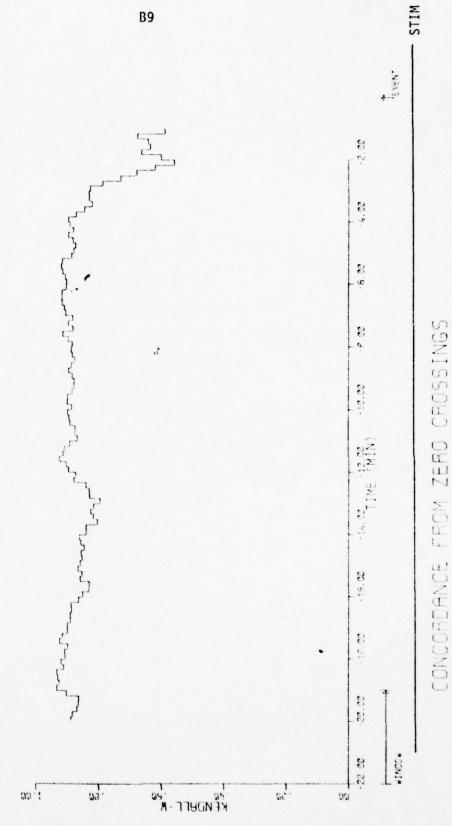
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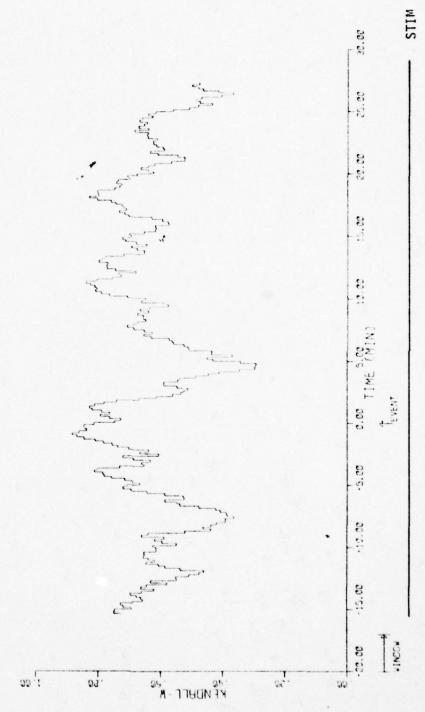
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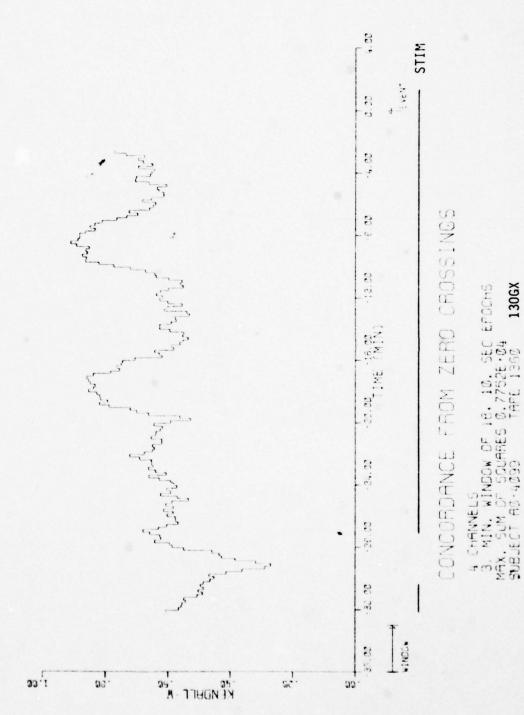


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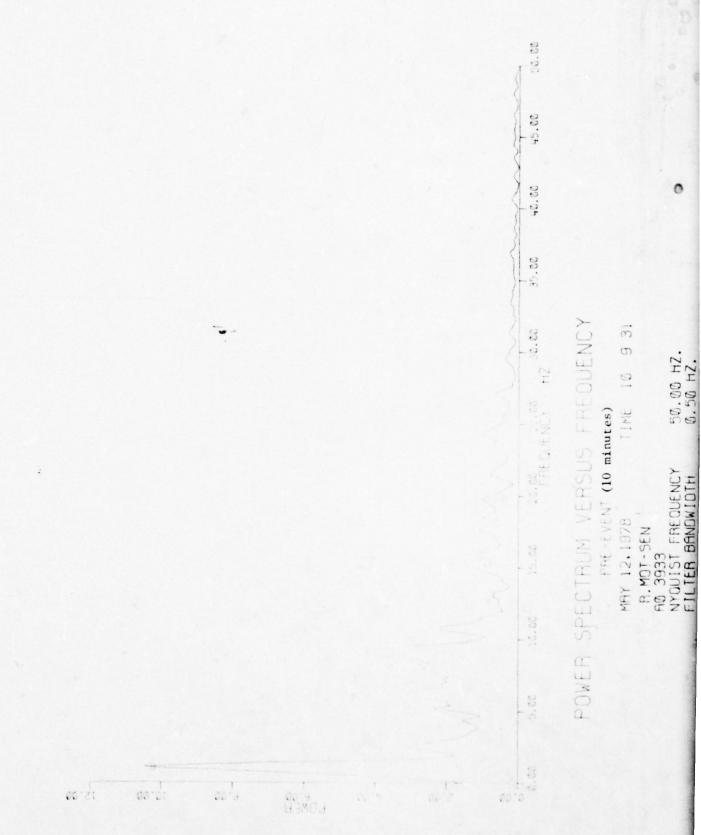
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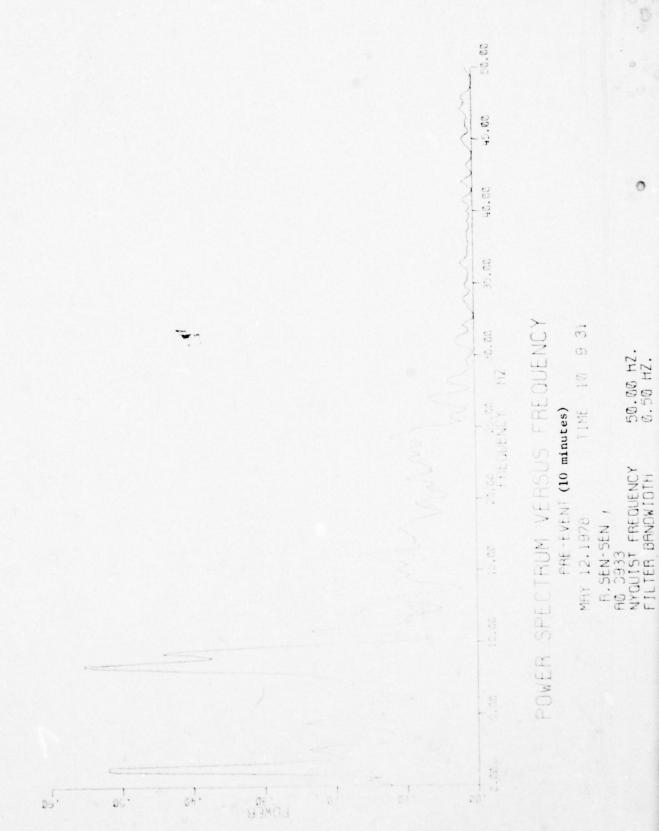


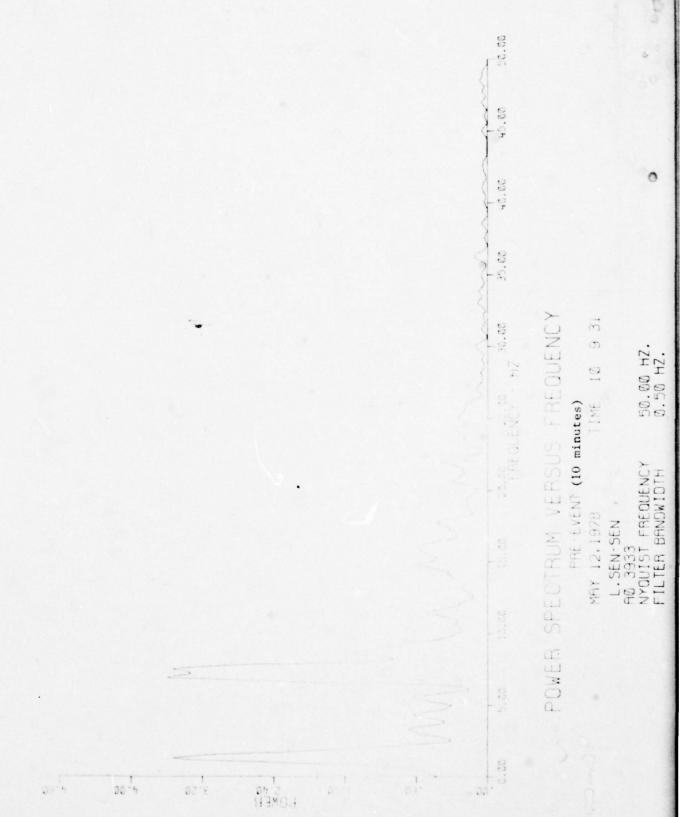
Figures C1 - C36

Power Spectral Density Plots

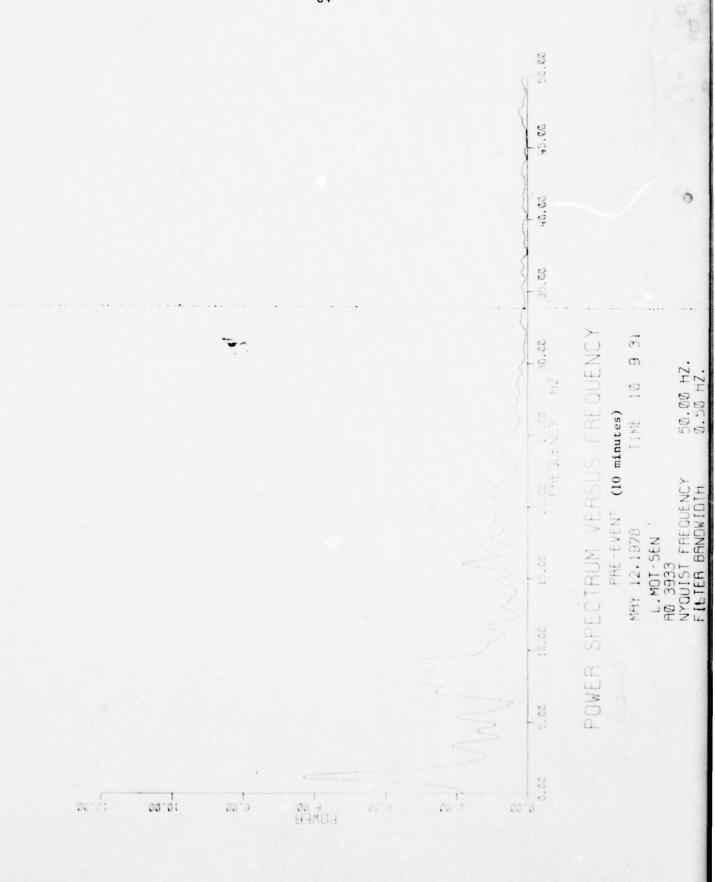
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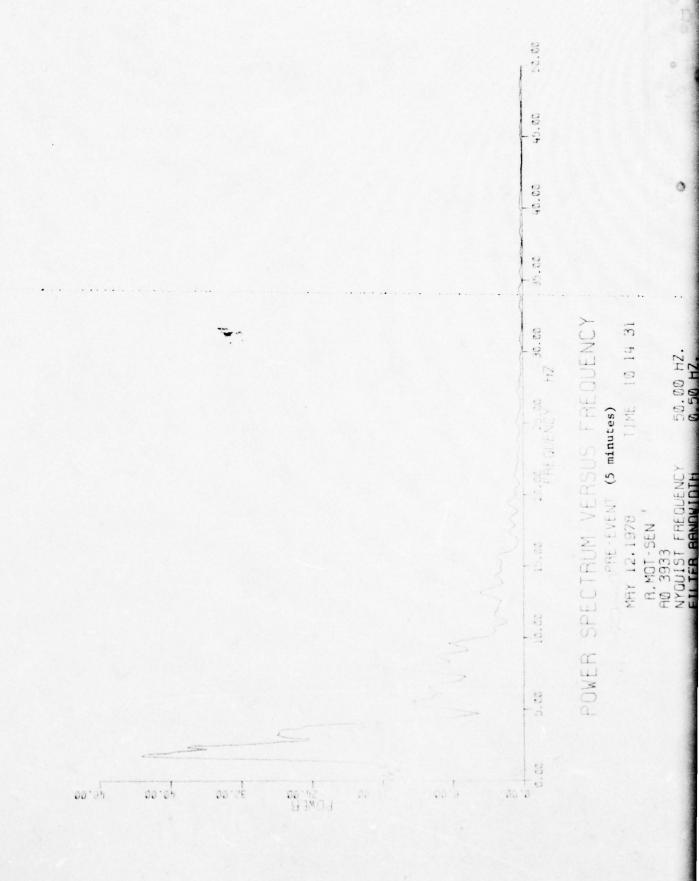


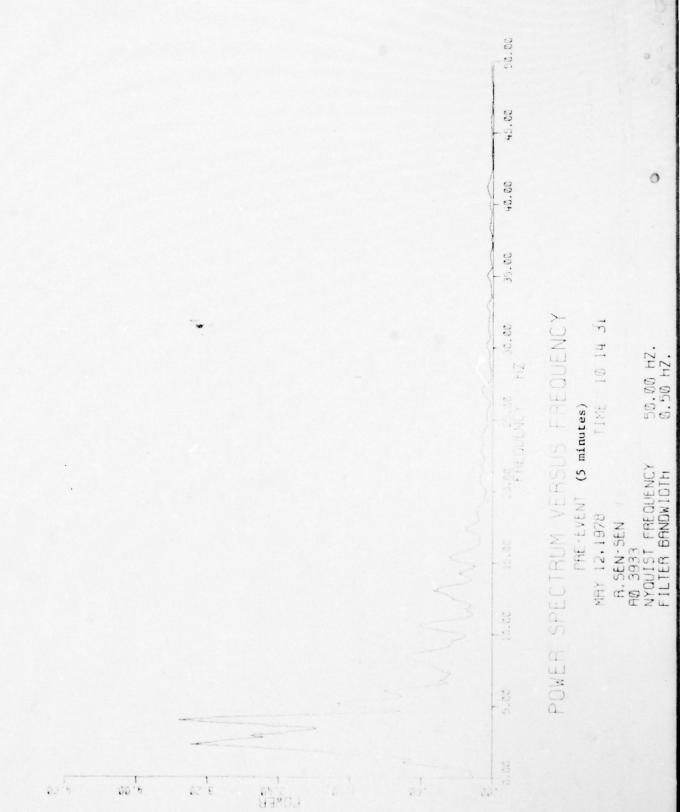


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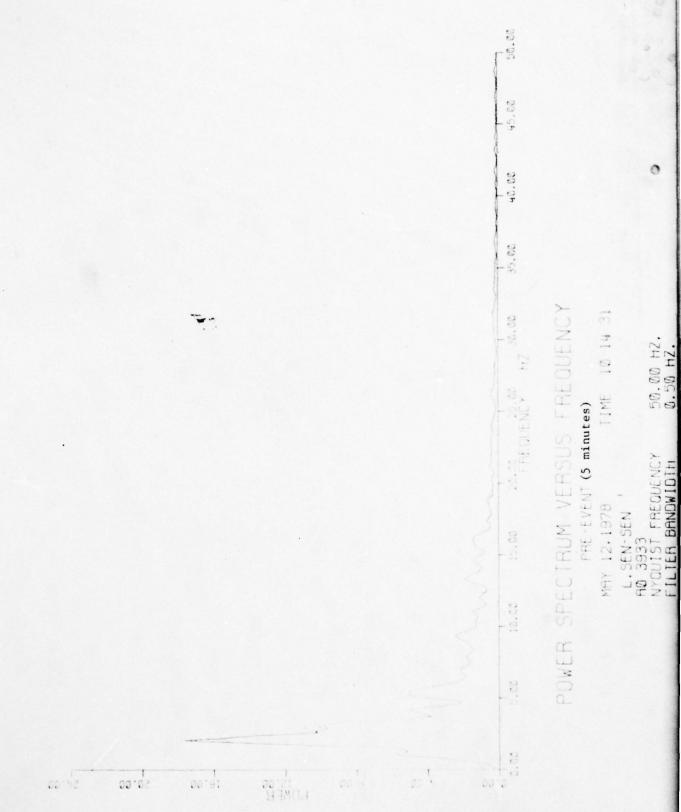
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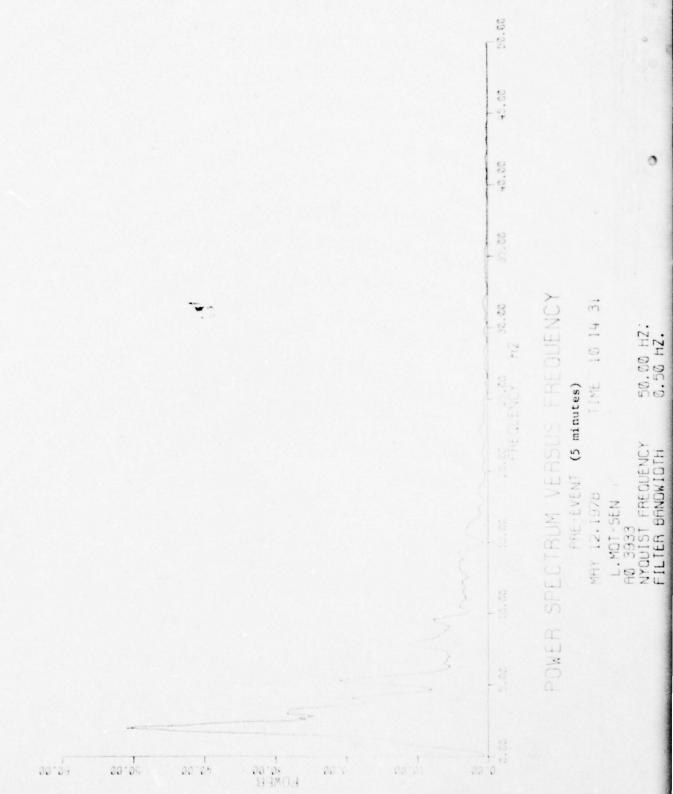


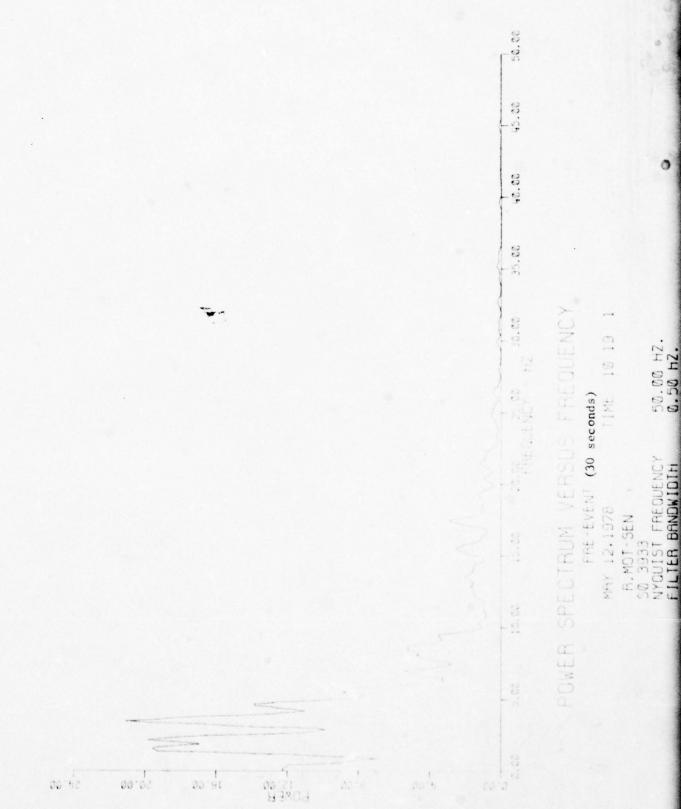


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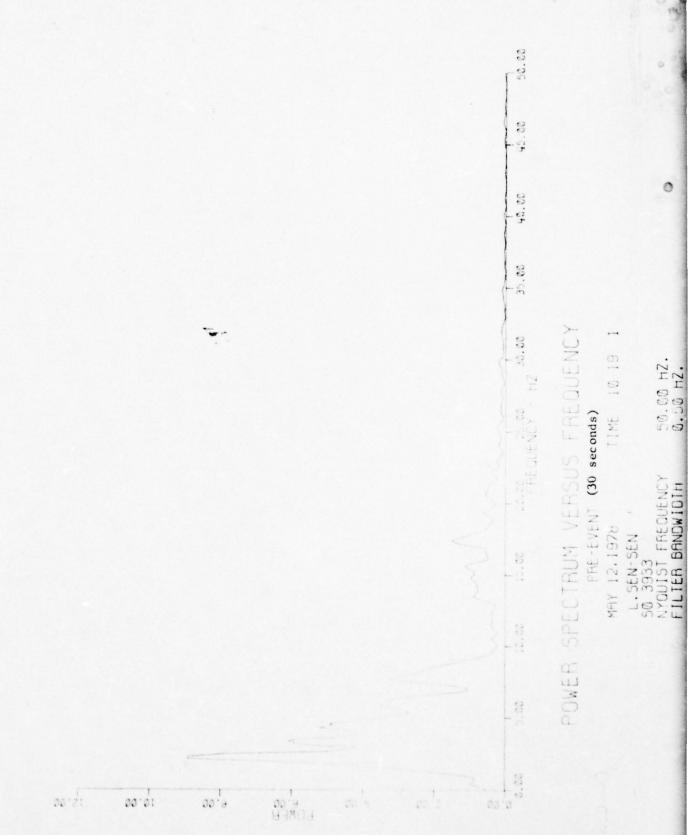


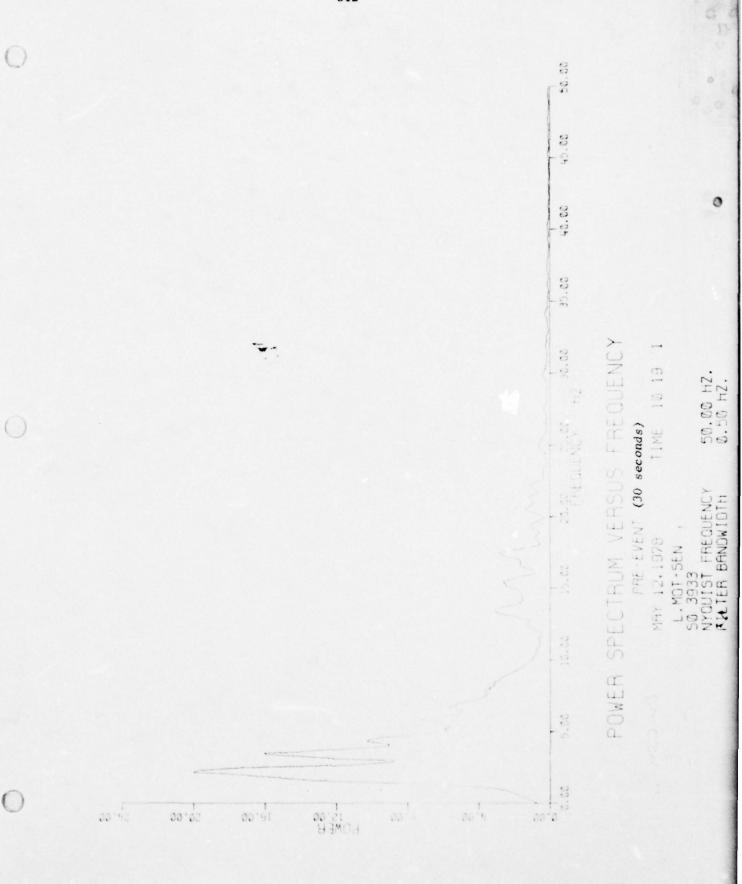


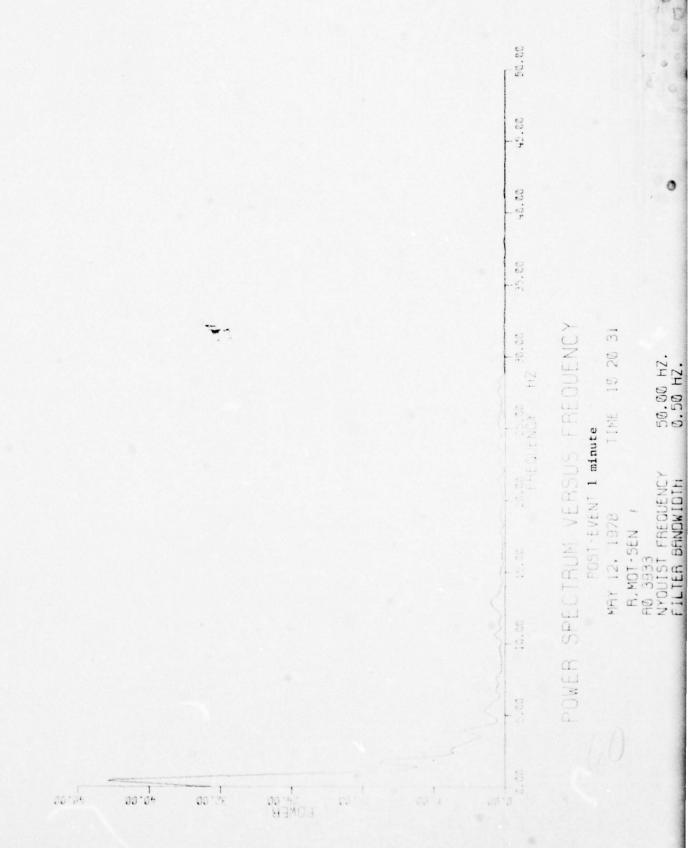


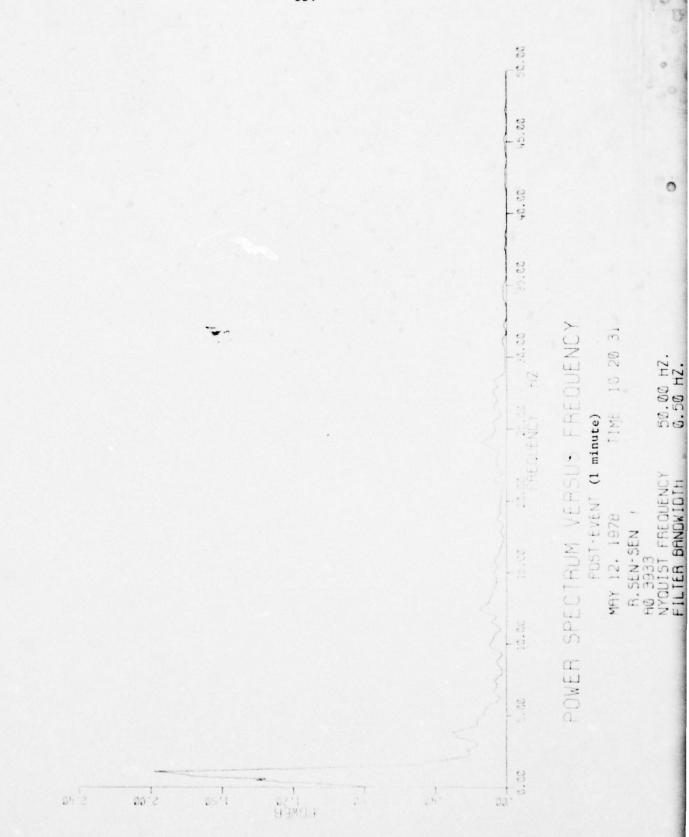
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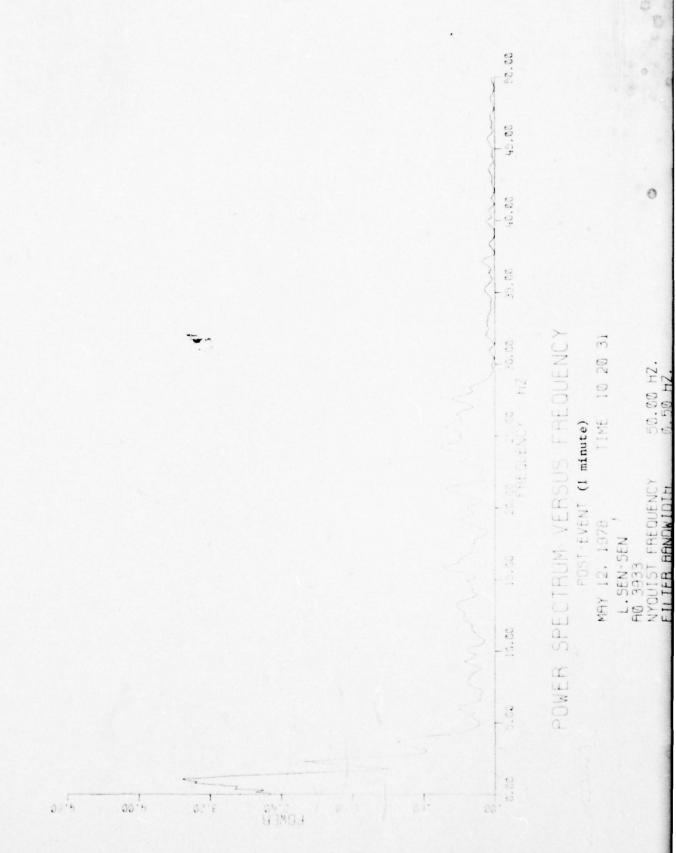
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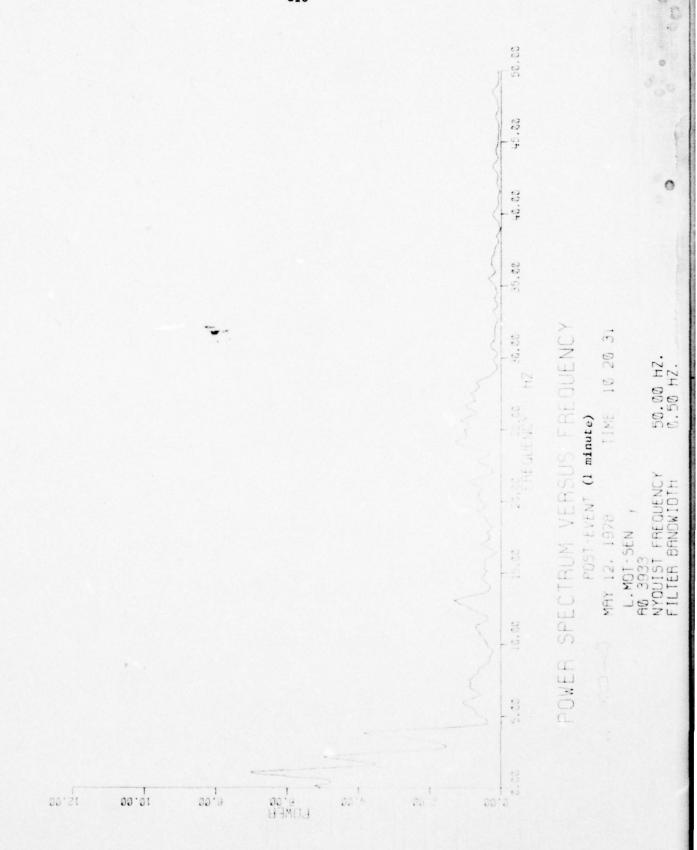


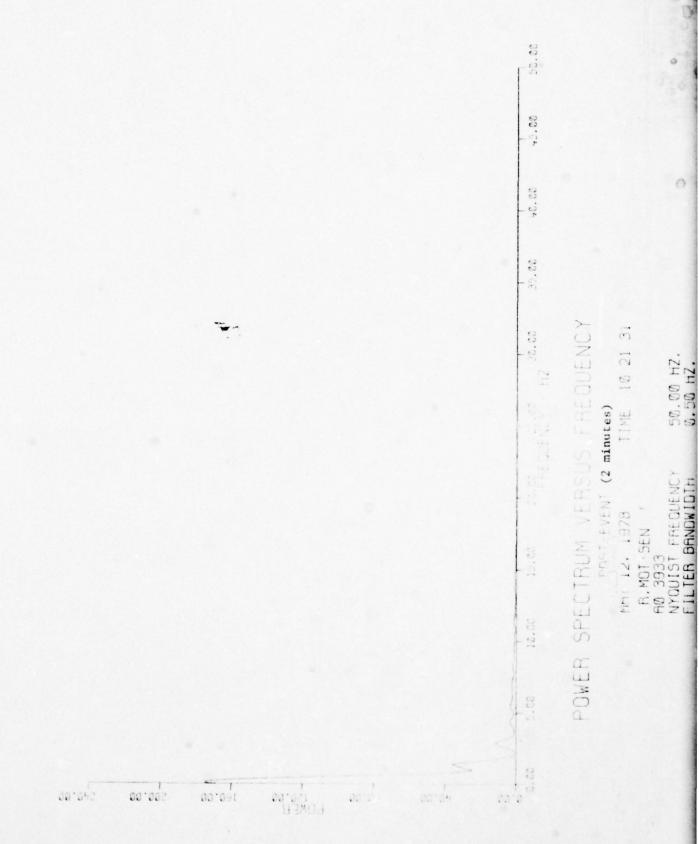




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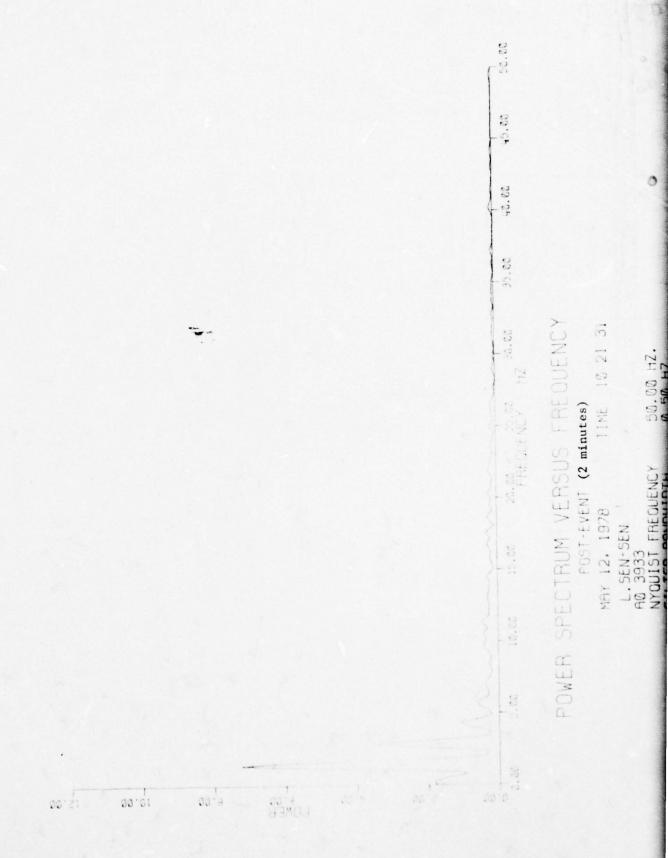
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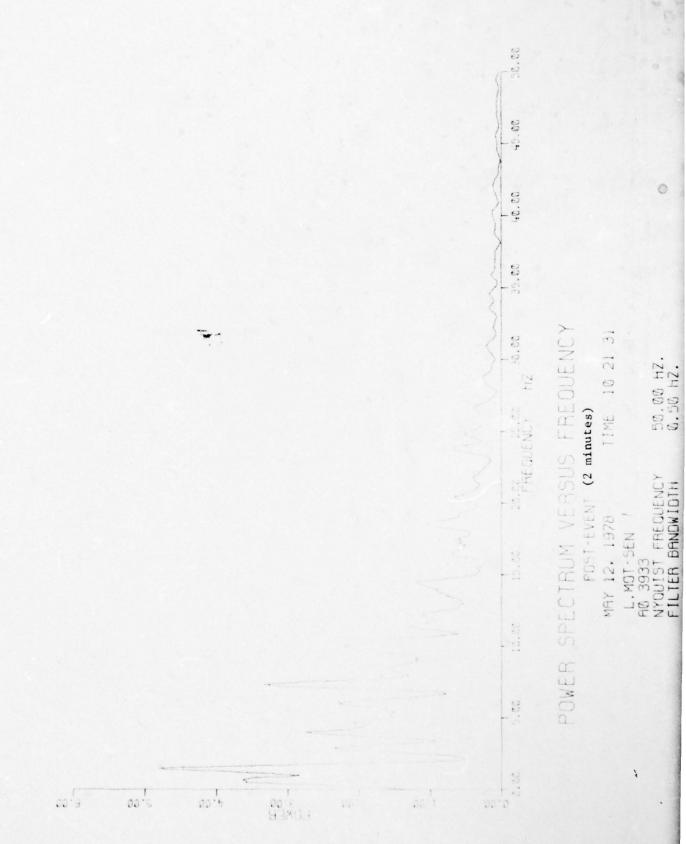
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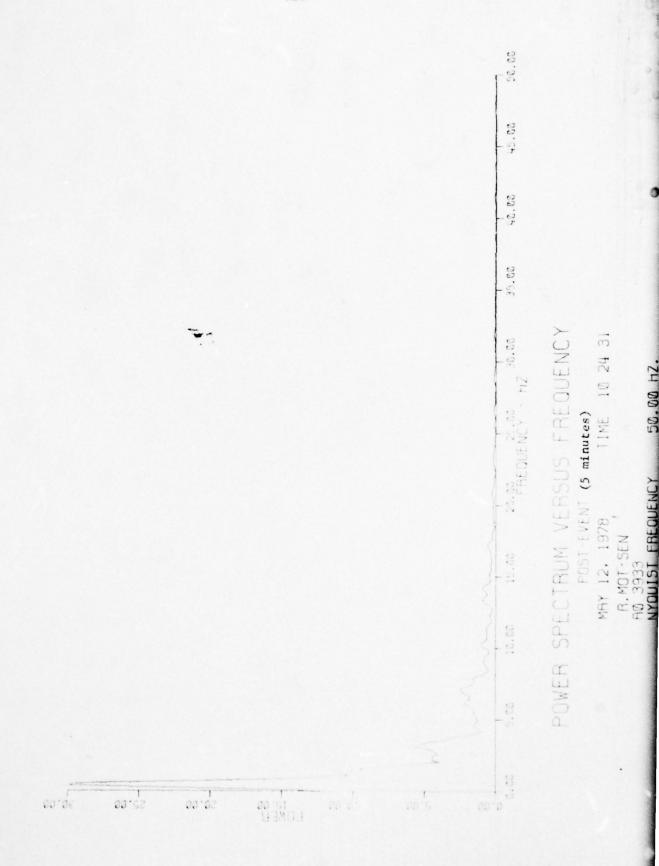
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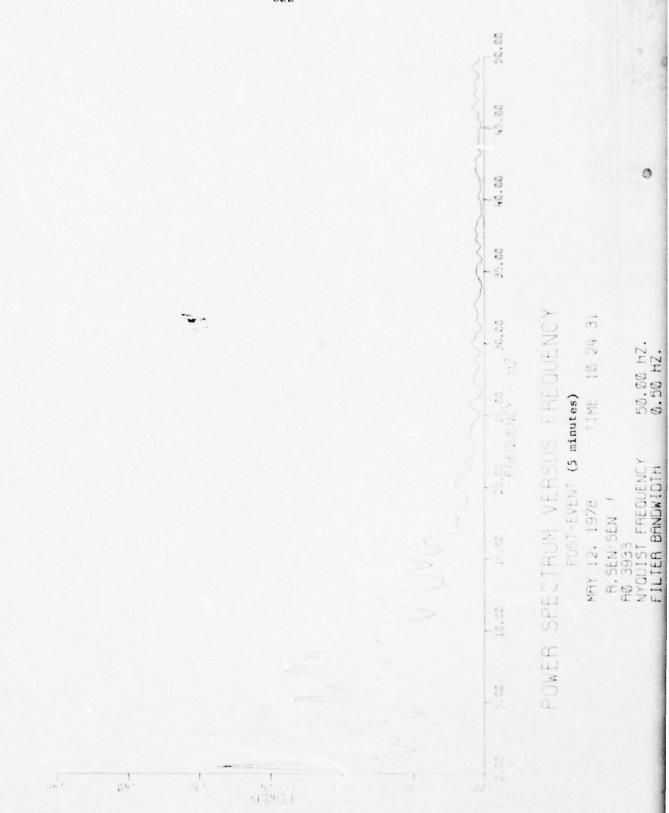




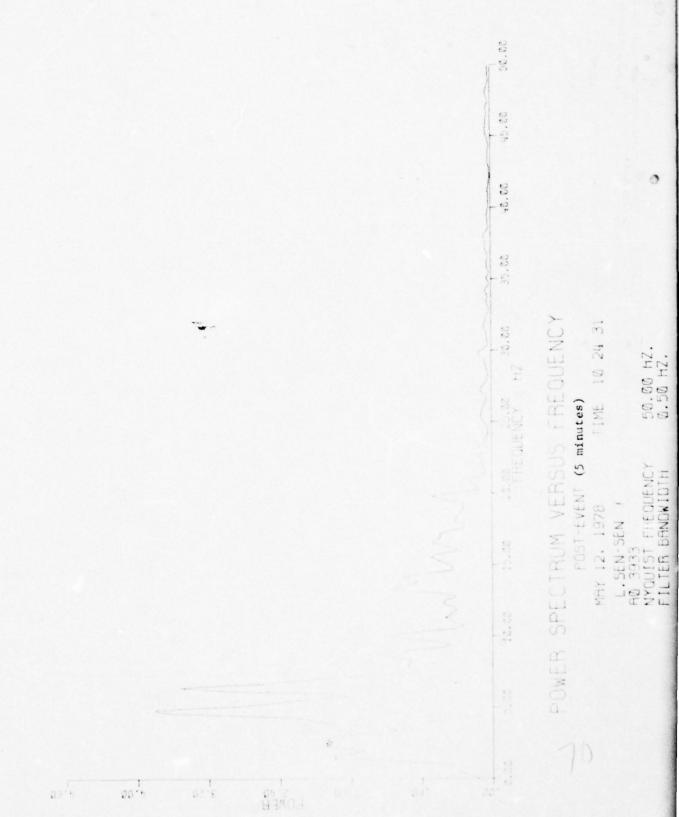


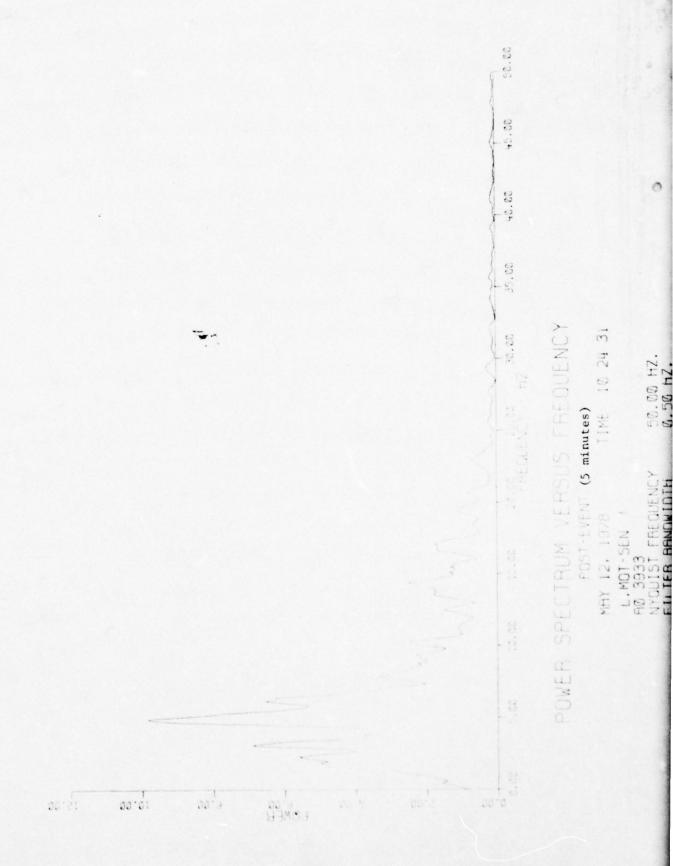
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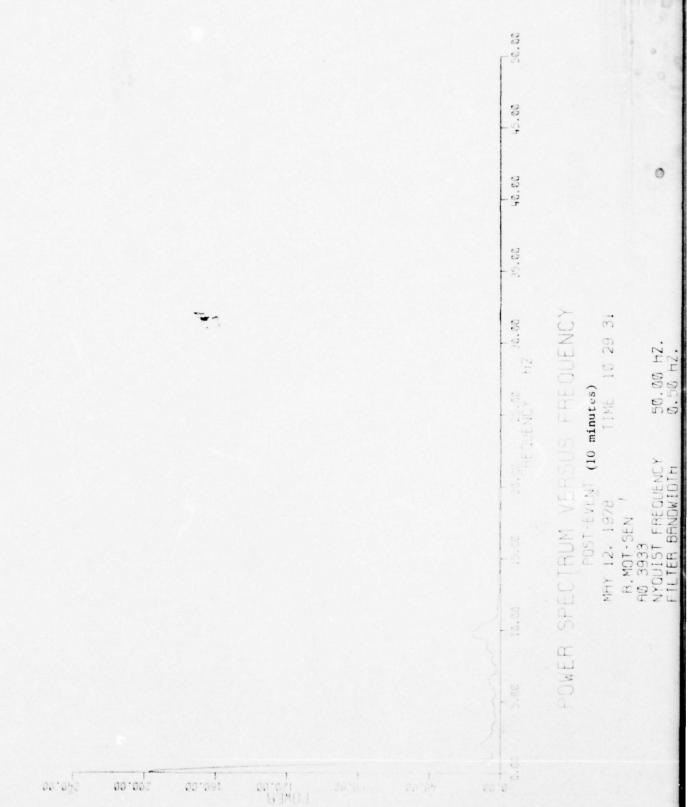


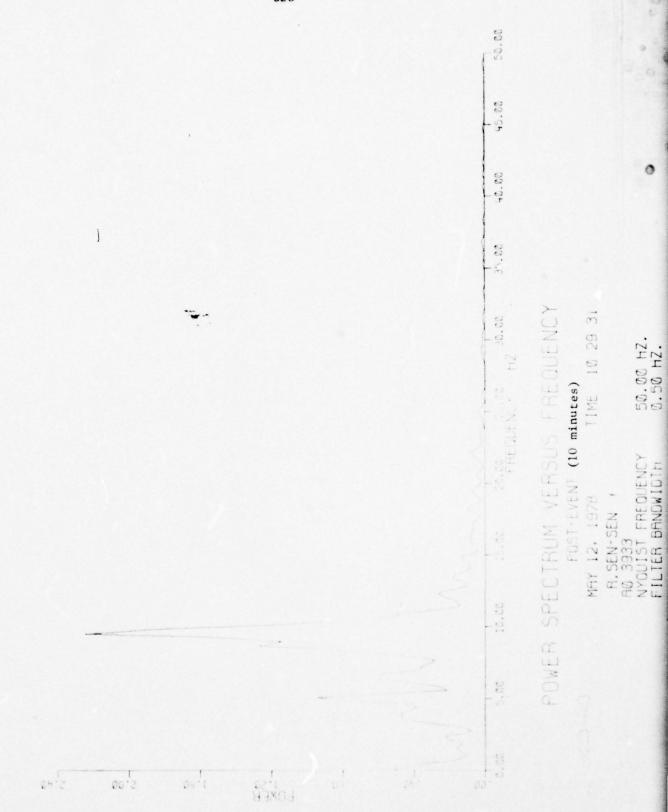


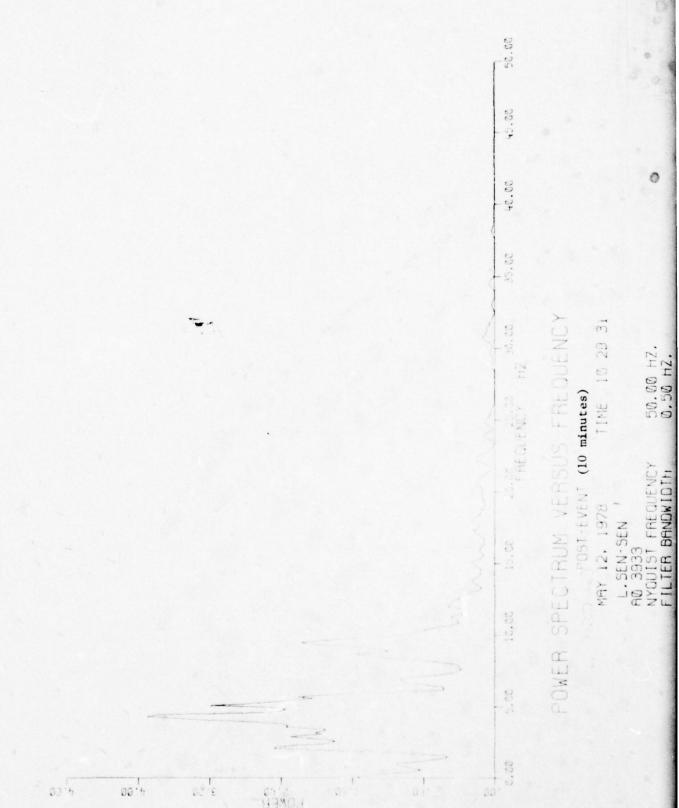
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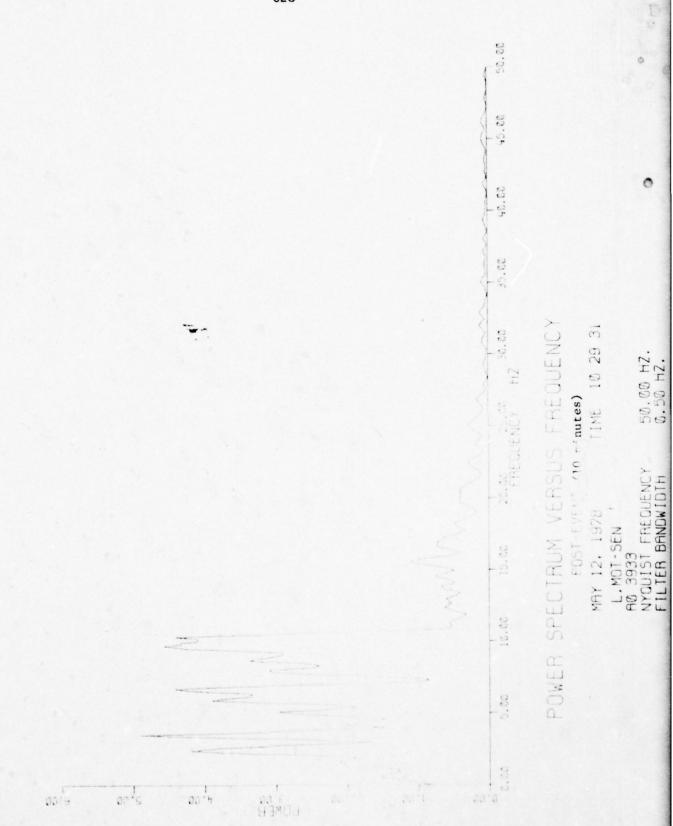


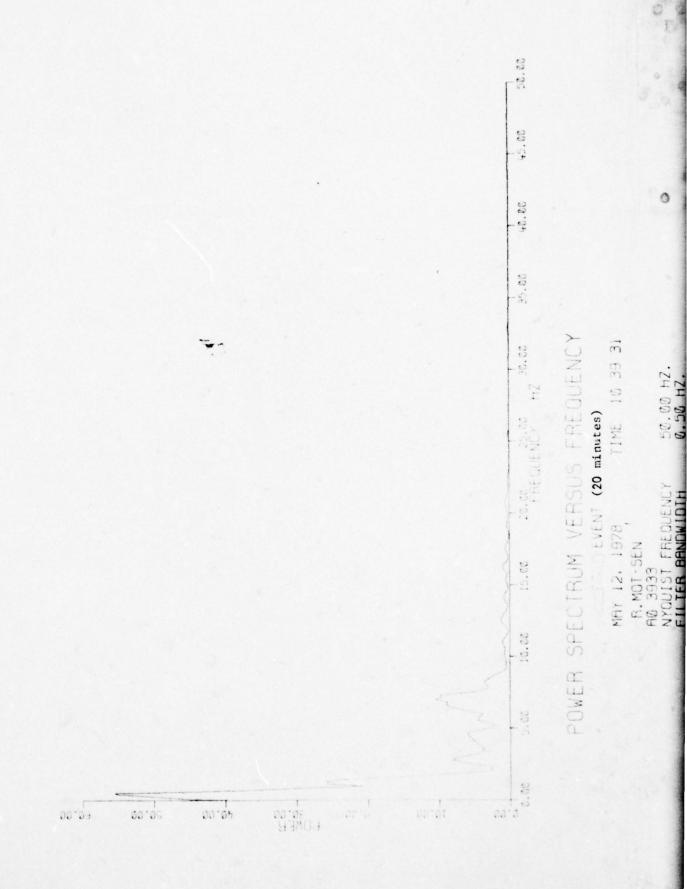


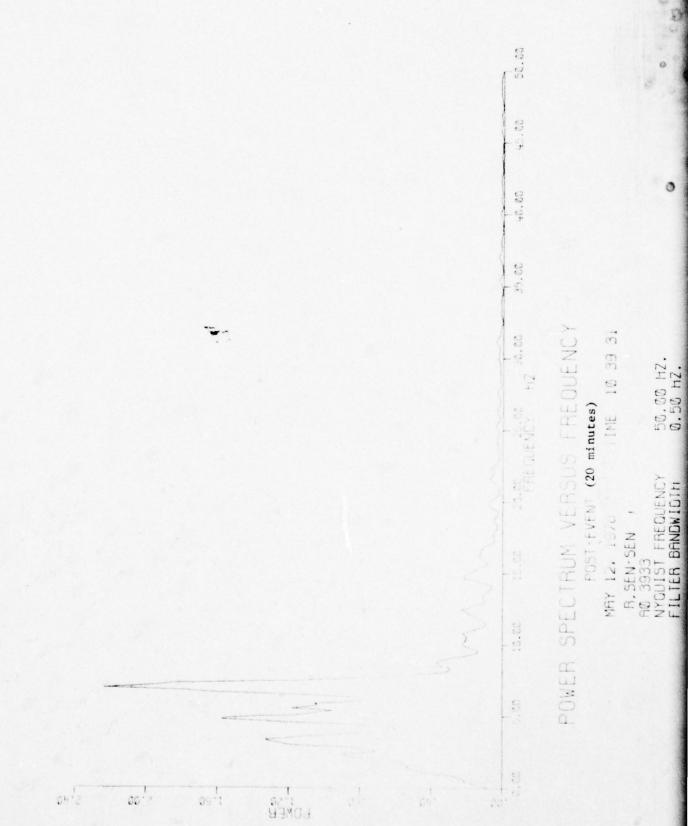




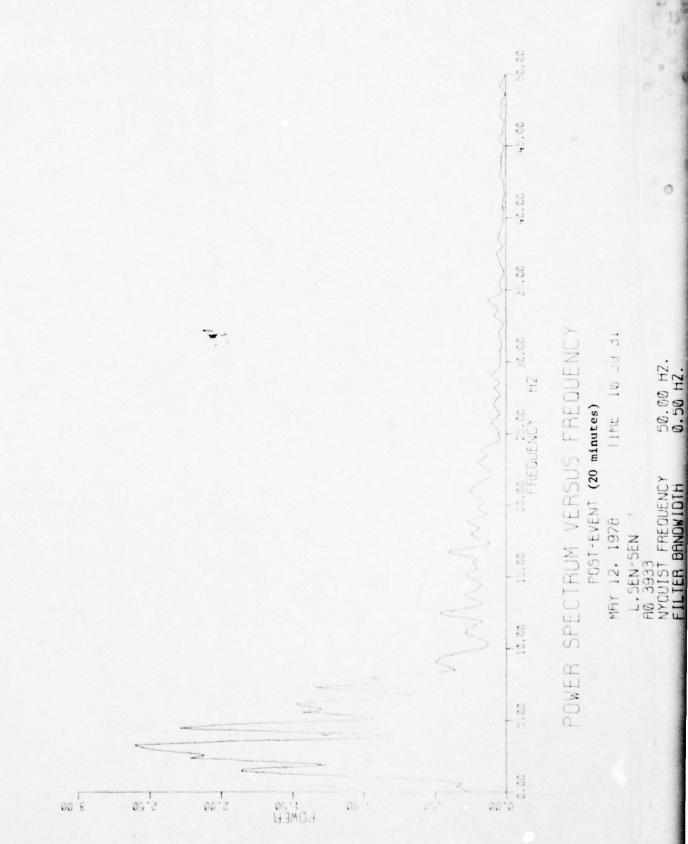


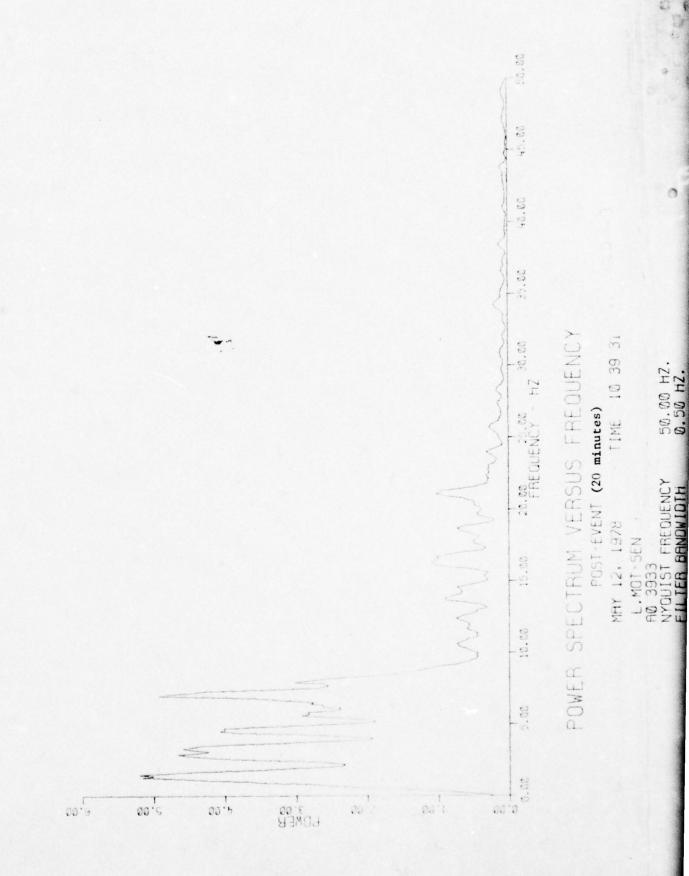


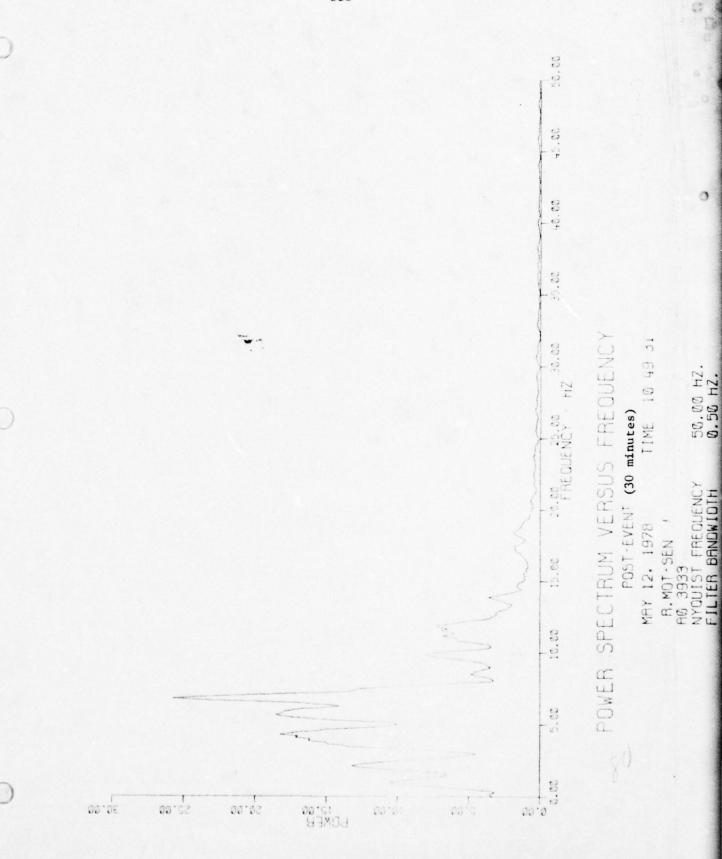


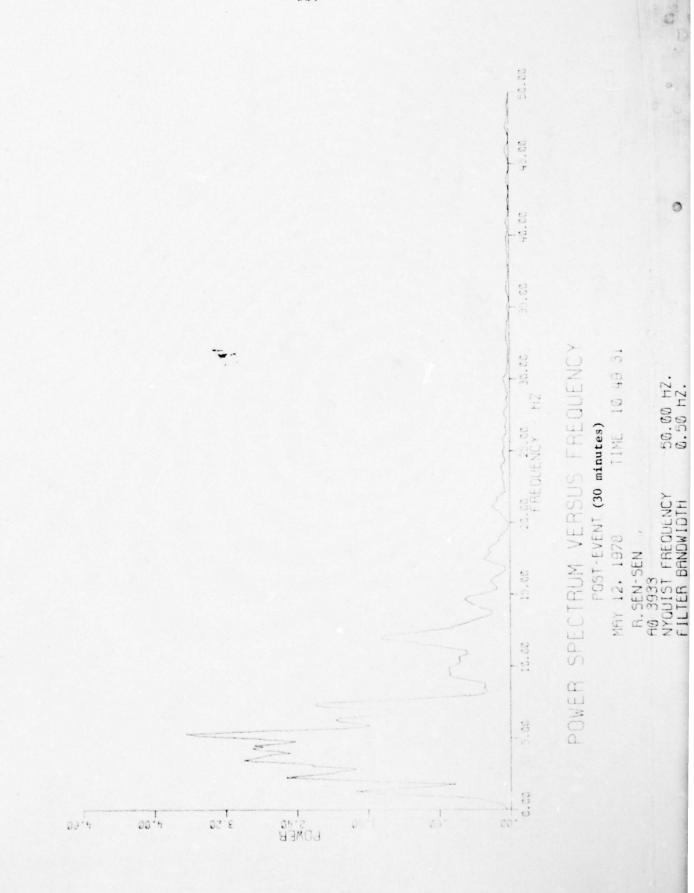


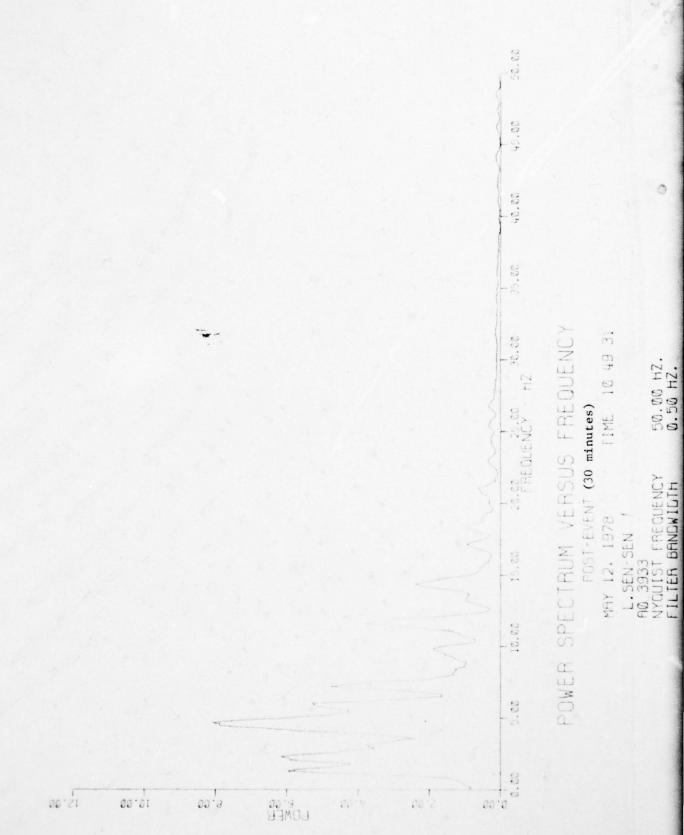
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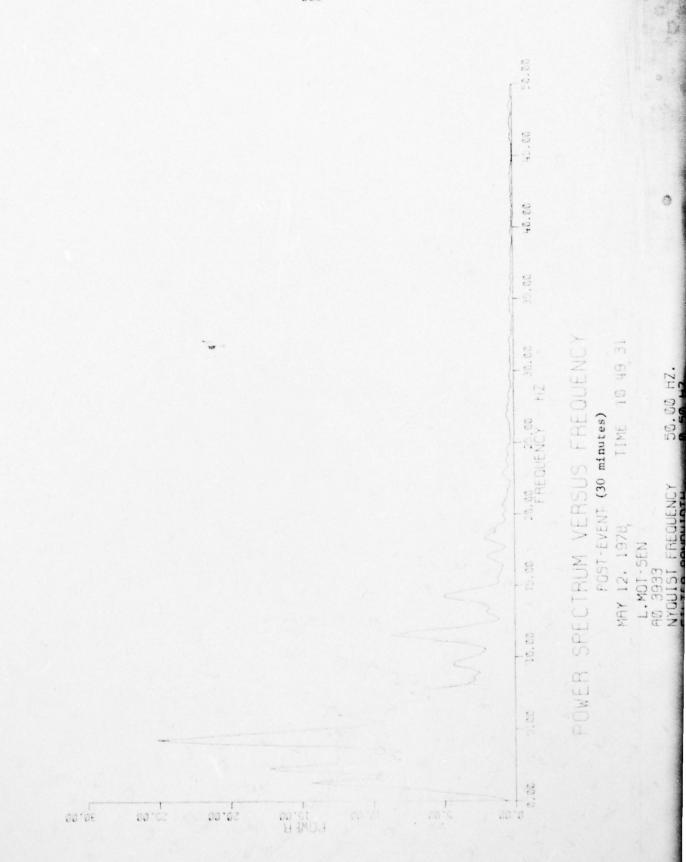












Figures D1 - D36

Evoked Potential Tracking Plots



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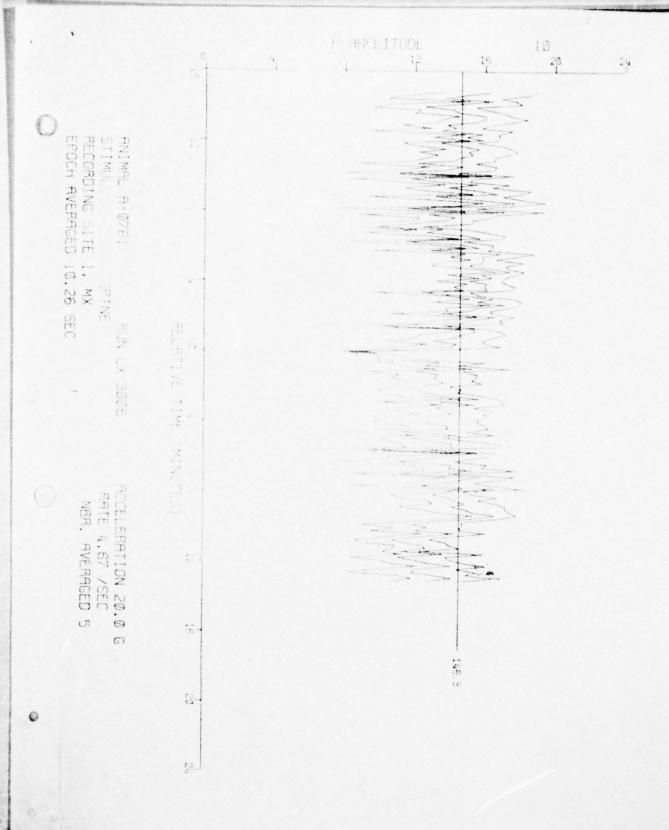
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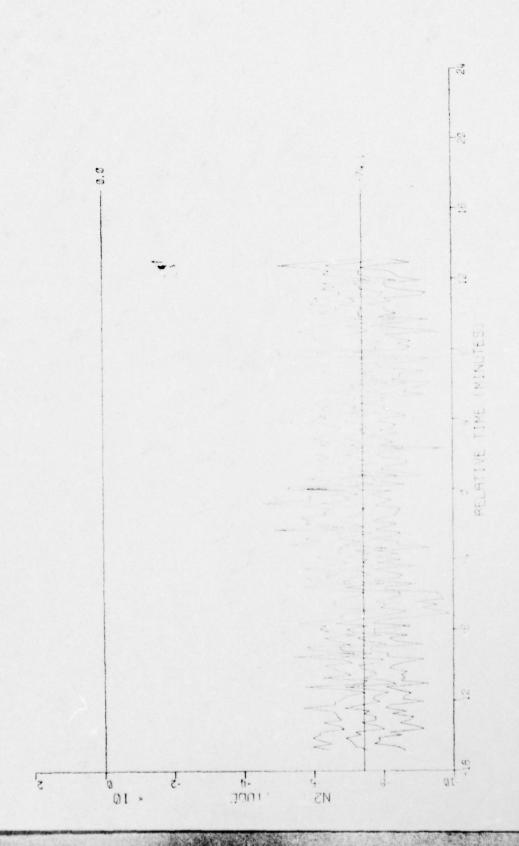


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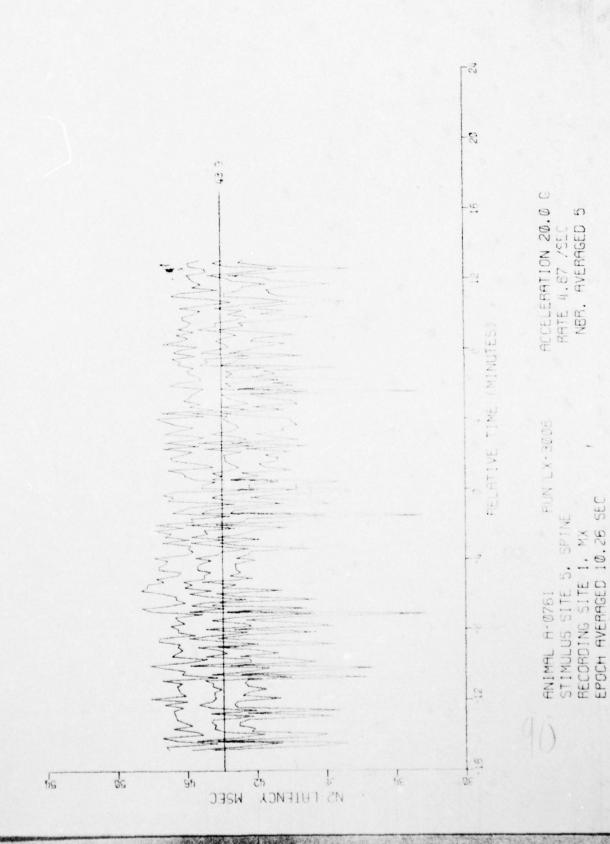


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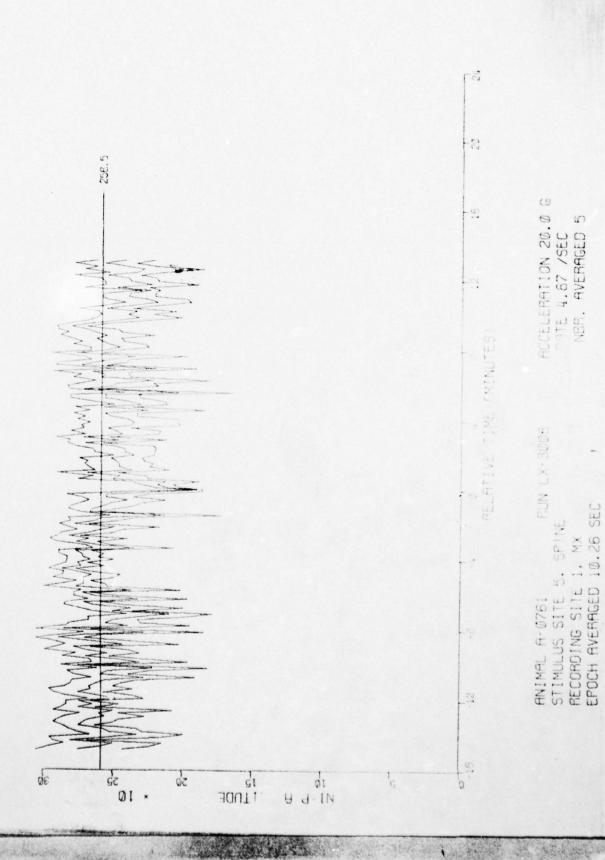
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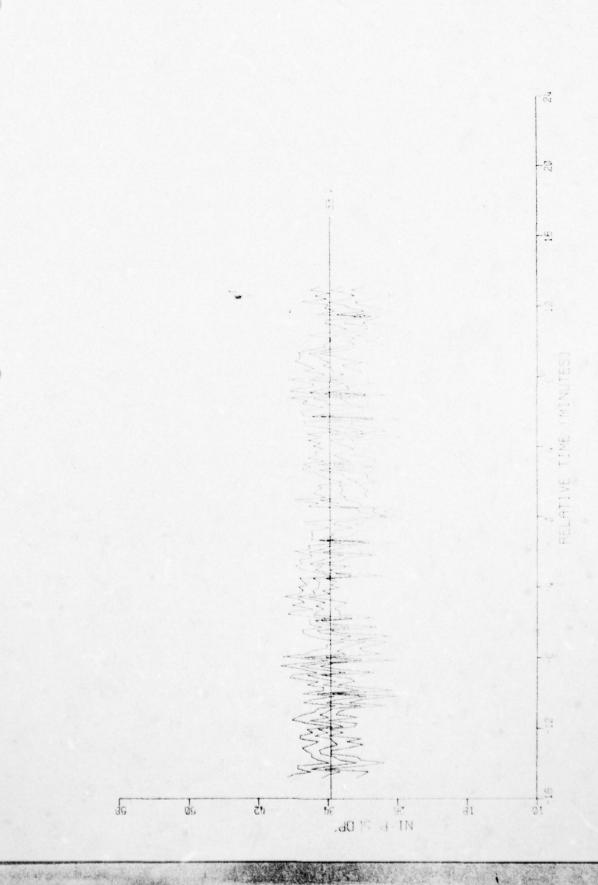
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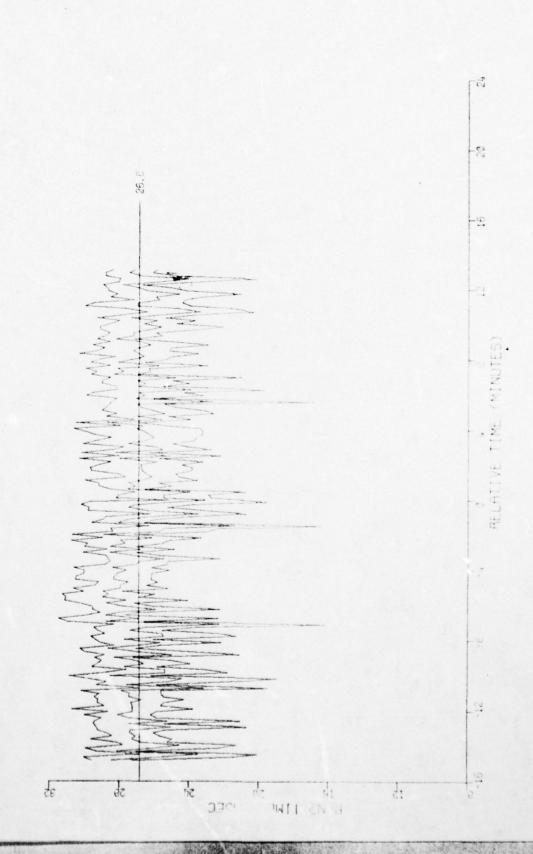
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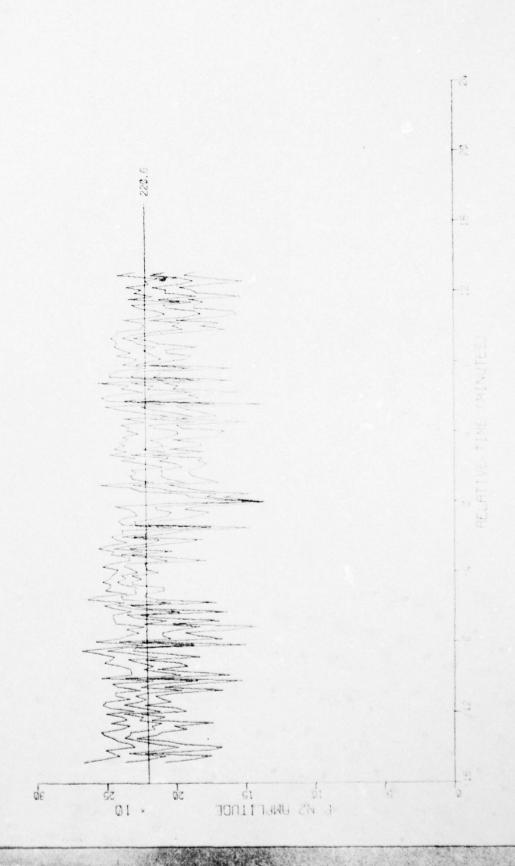
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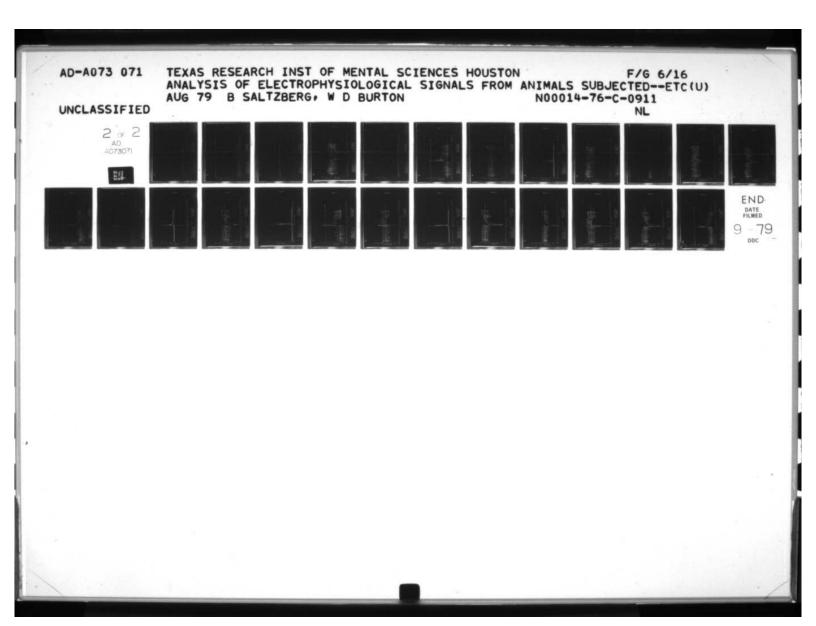
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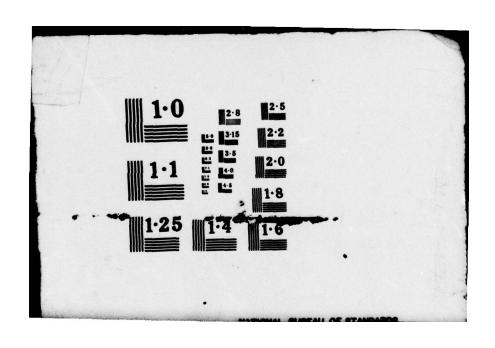
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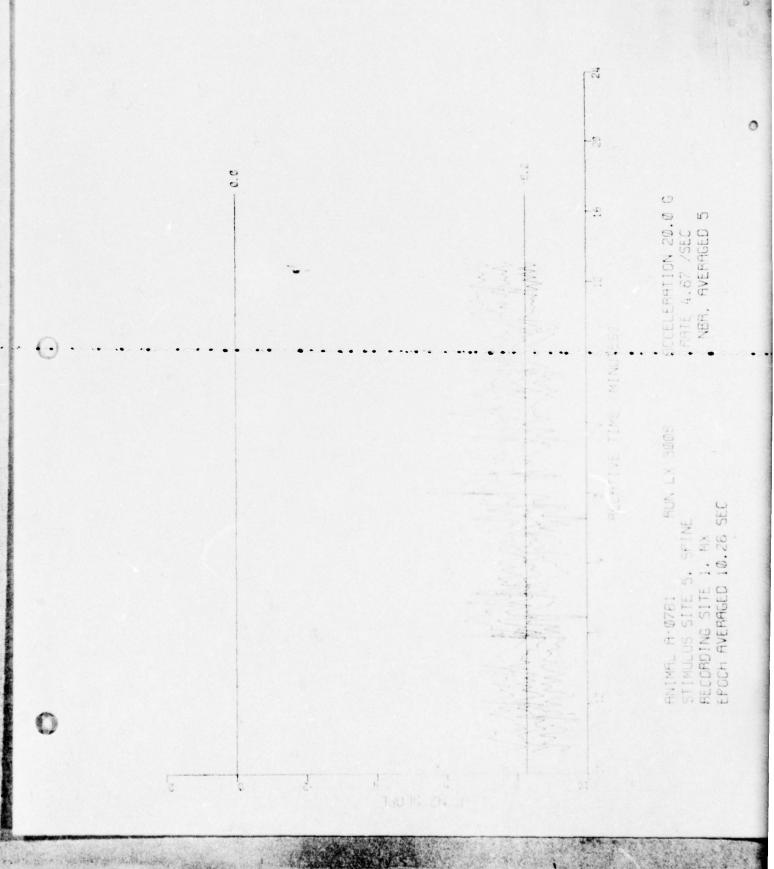


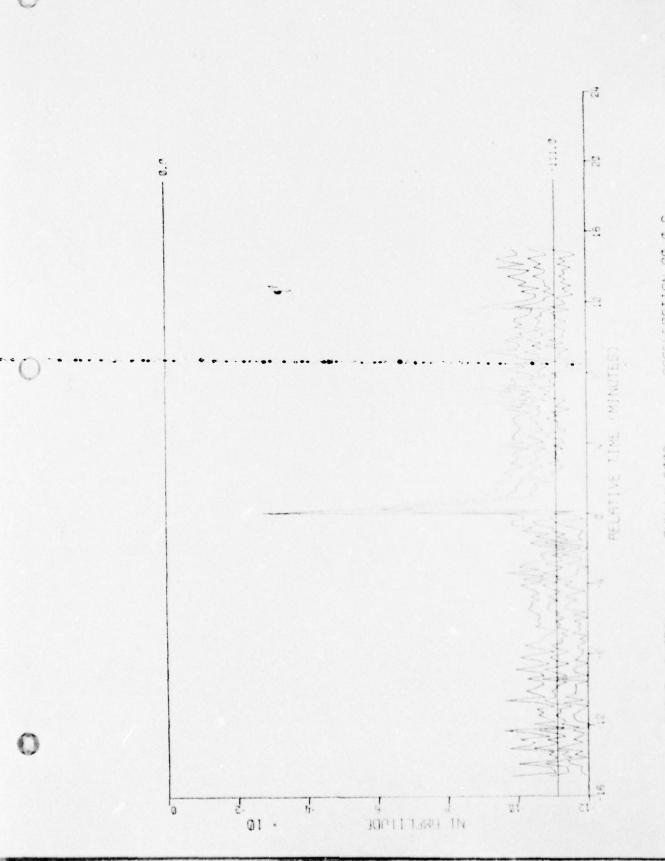
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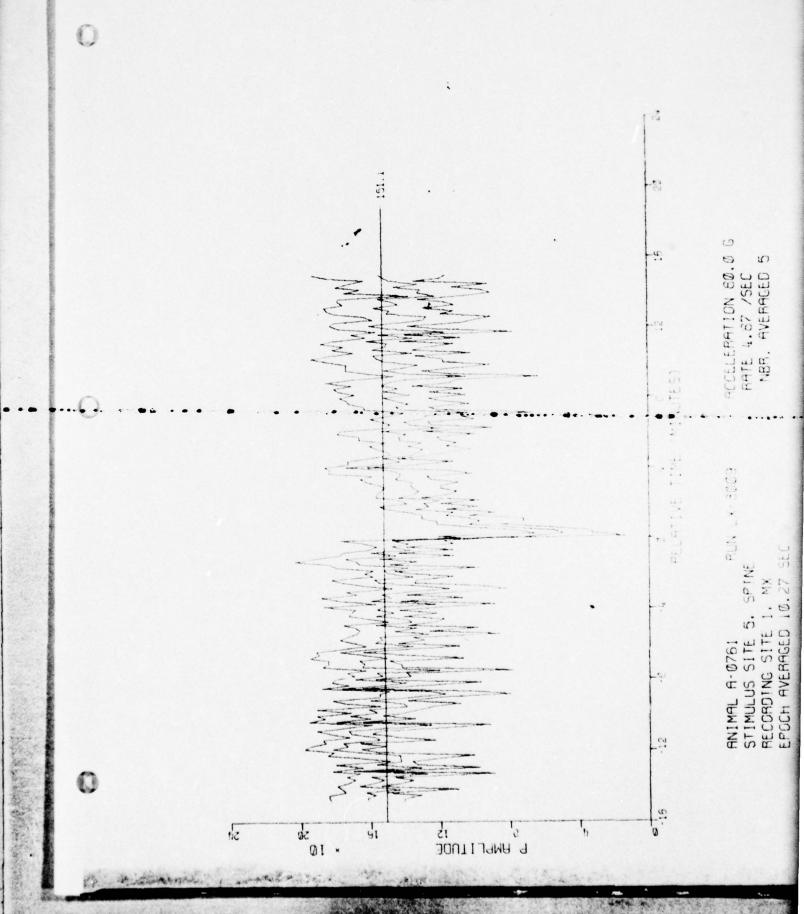
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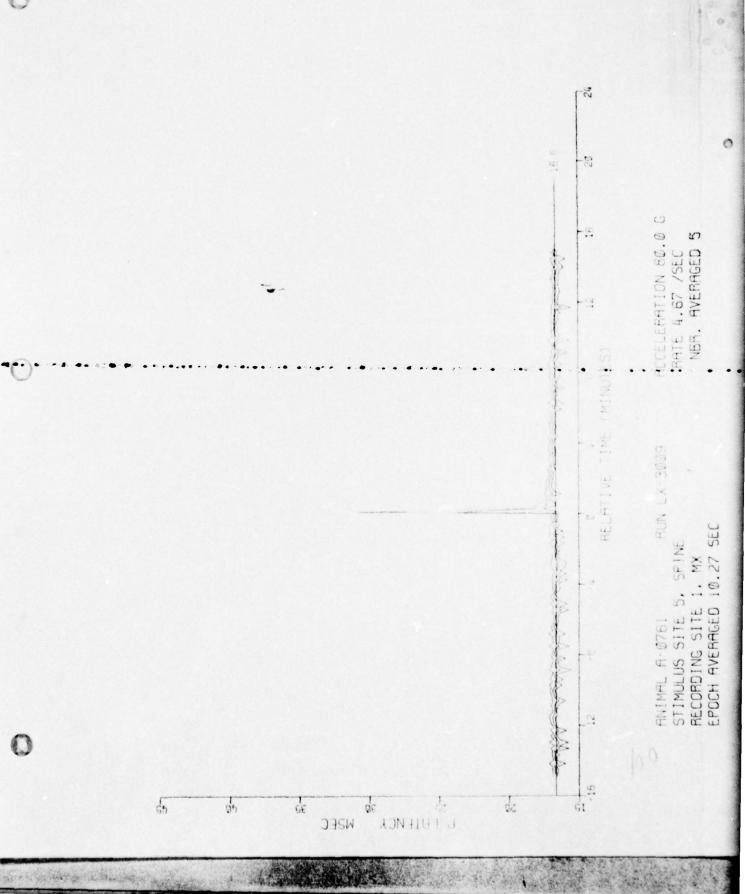


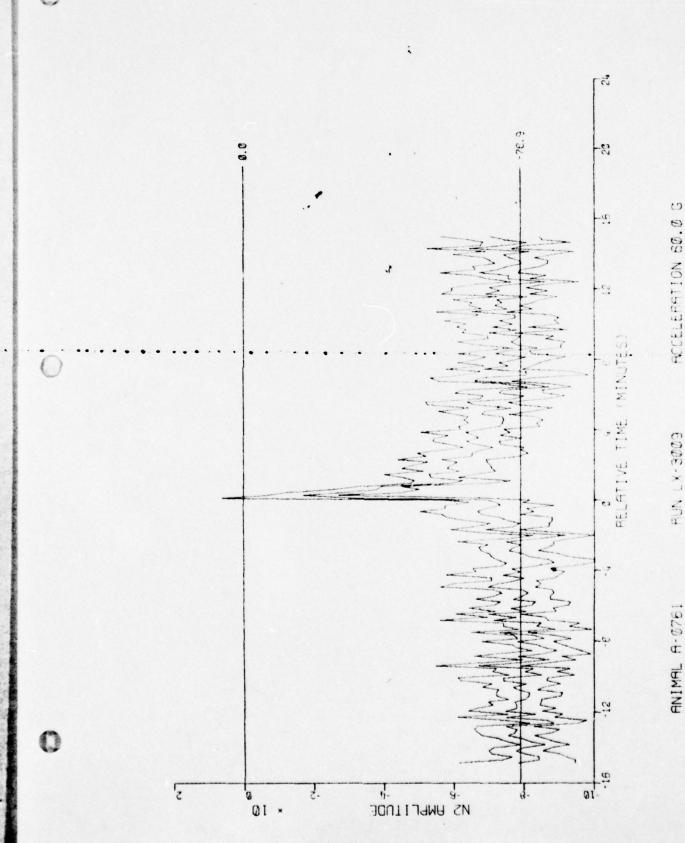
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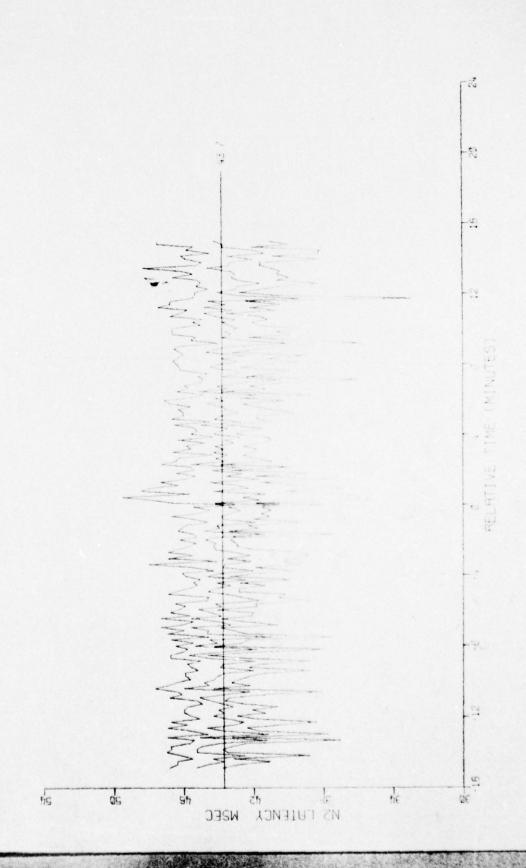
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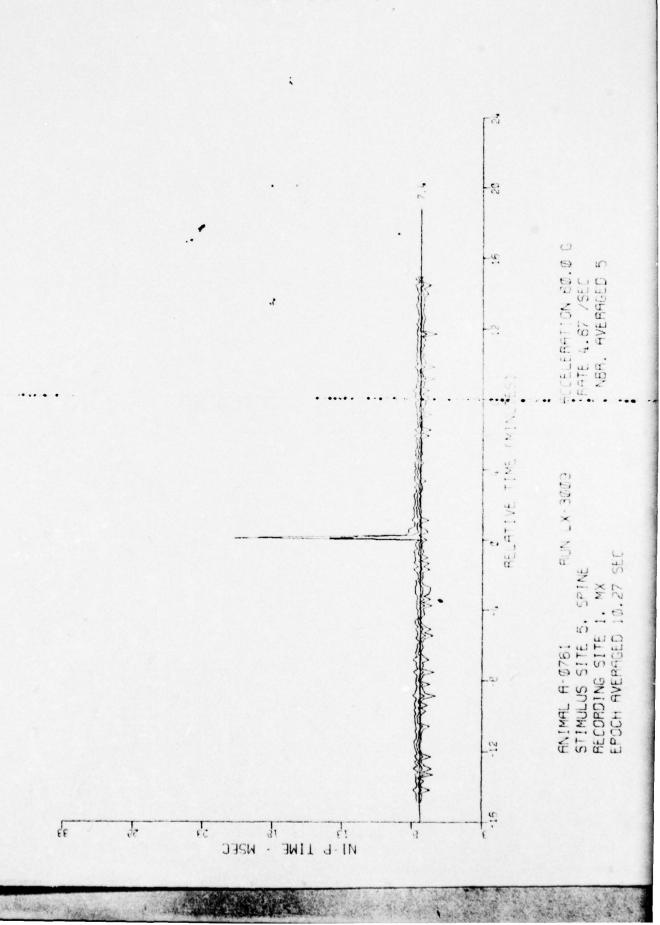


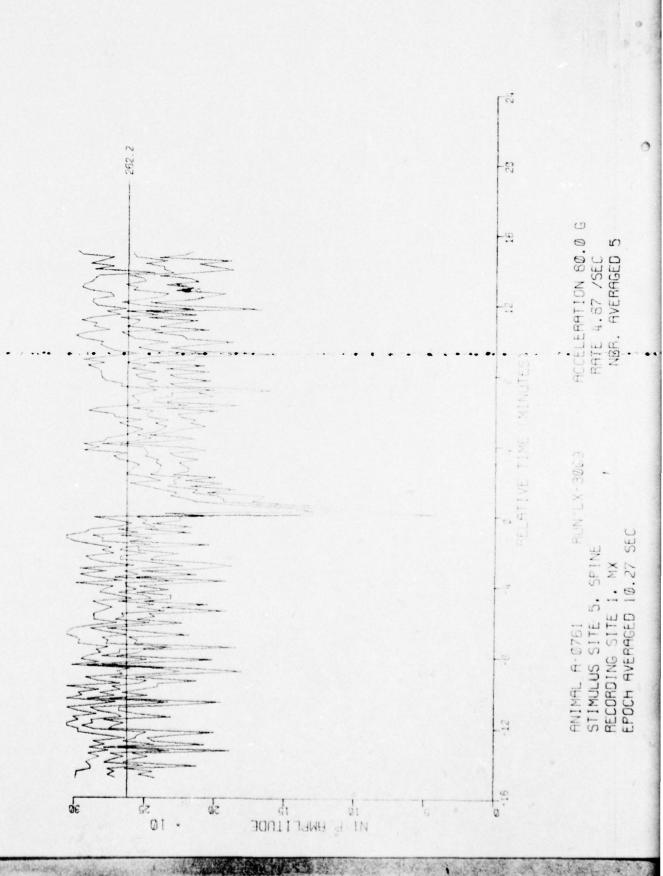
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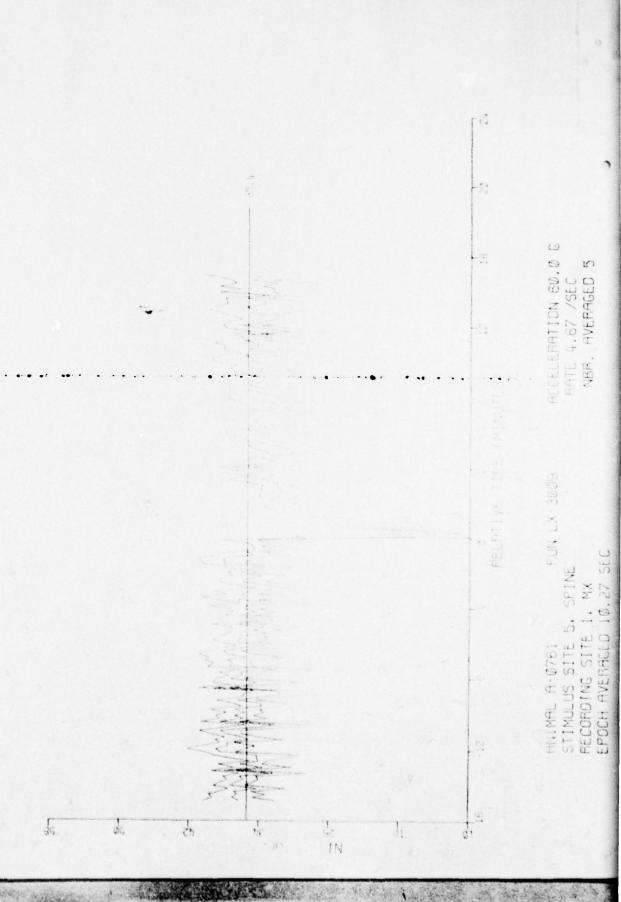


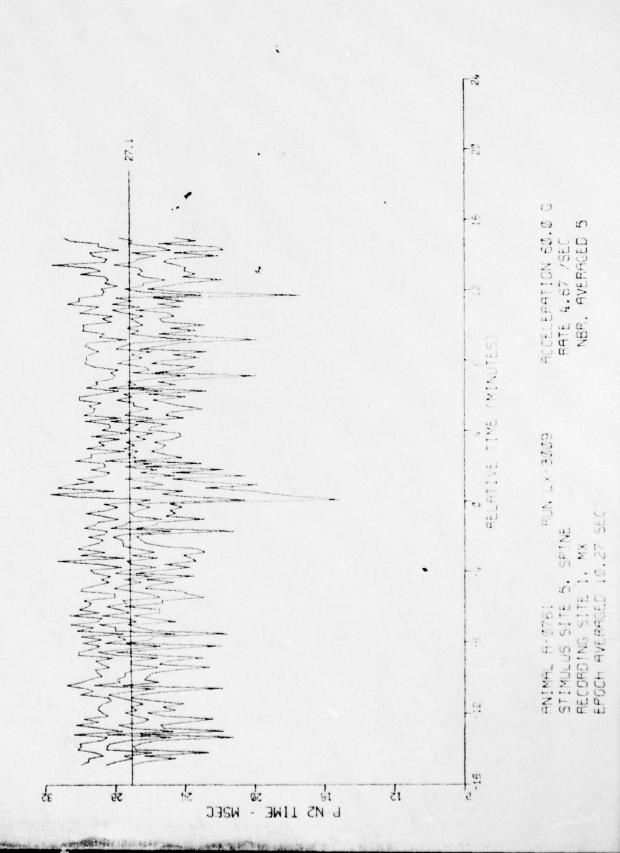
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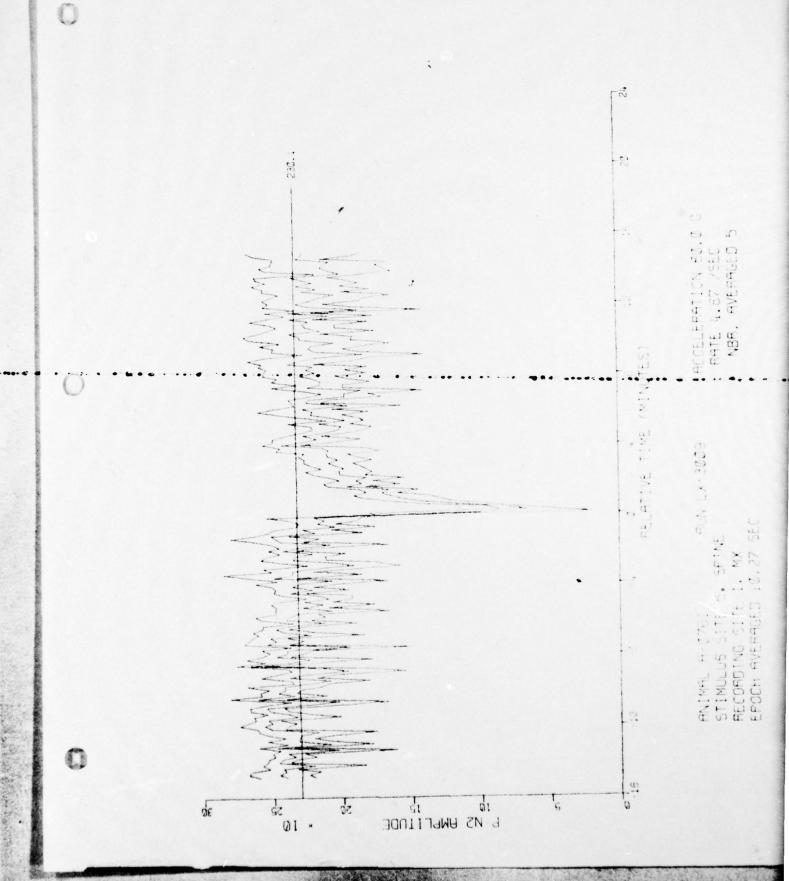
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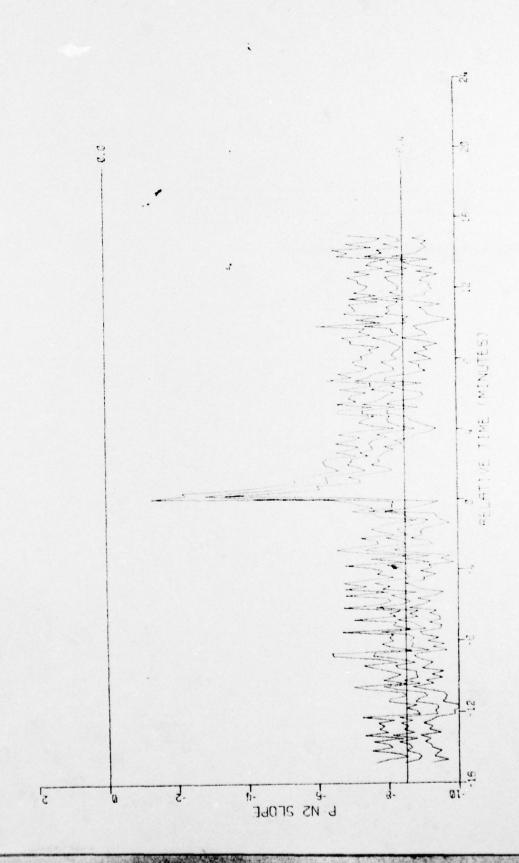




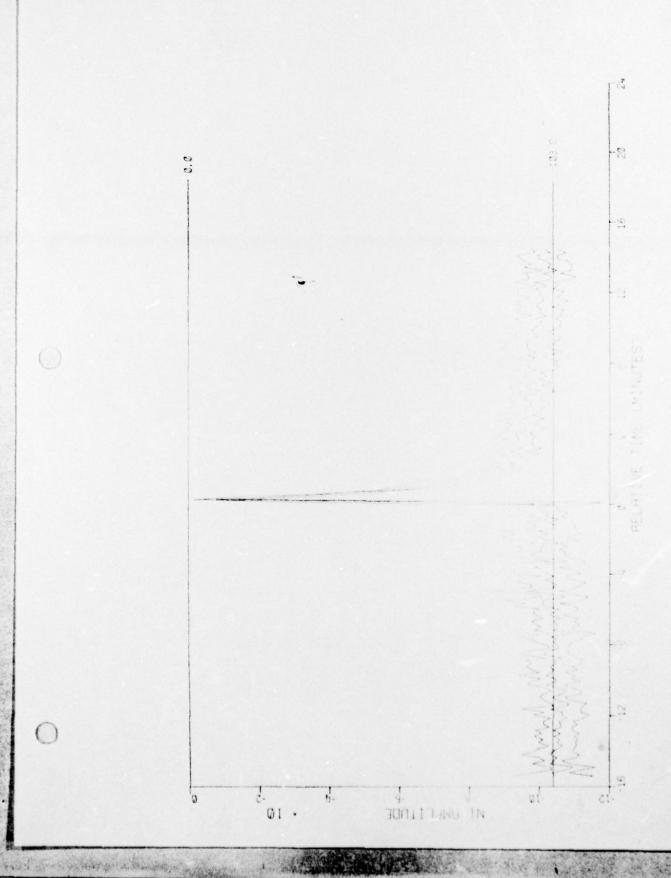








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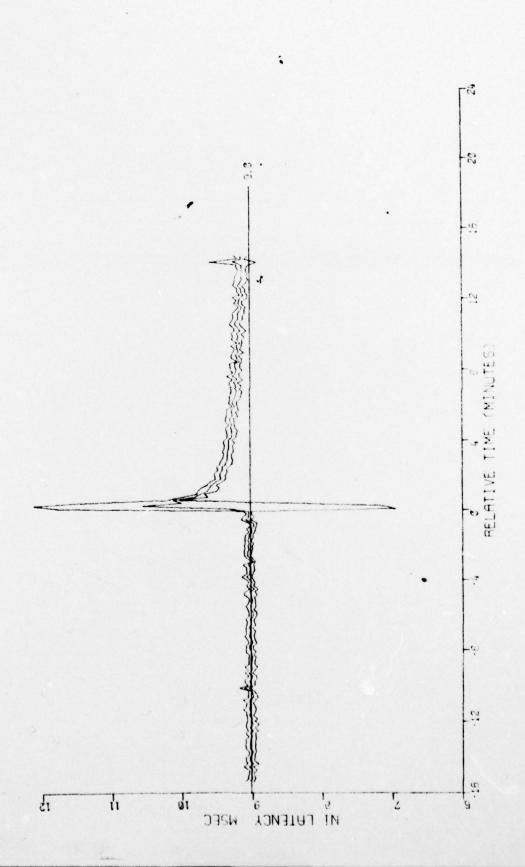


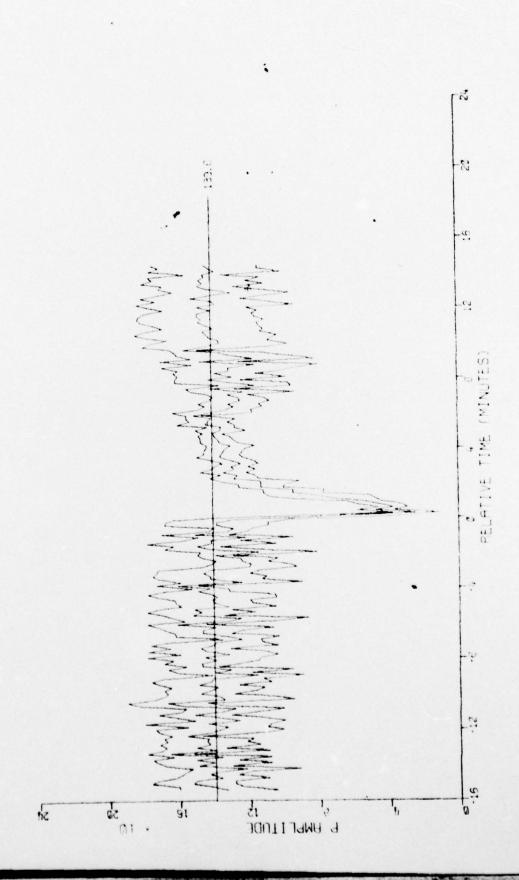
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ACCELERATION 100.0 G RATE 4.87 /SEC NBR. AVERAGED 5

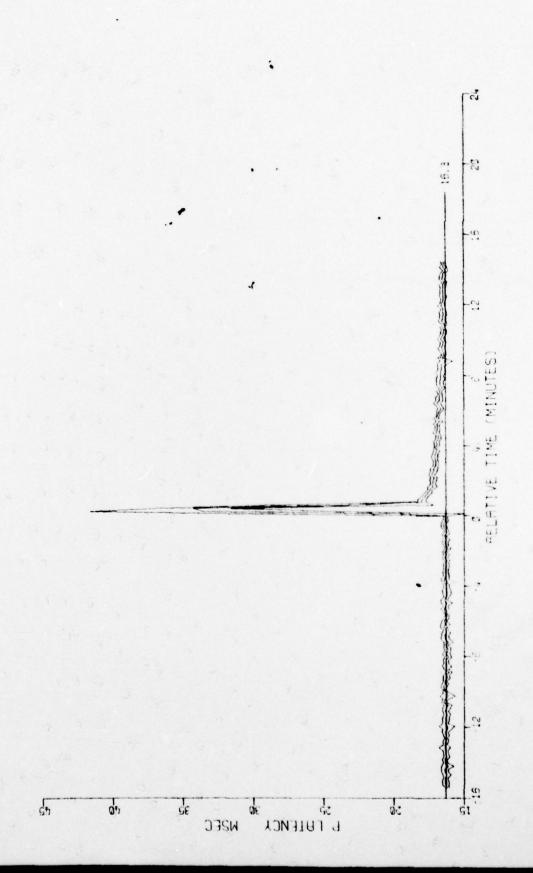
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EPOCH AVERAGED 10.26 SEC



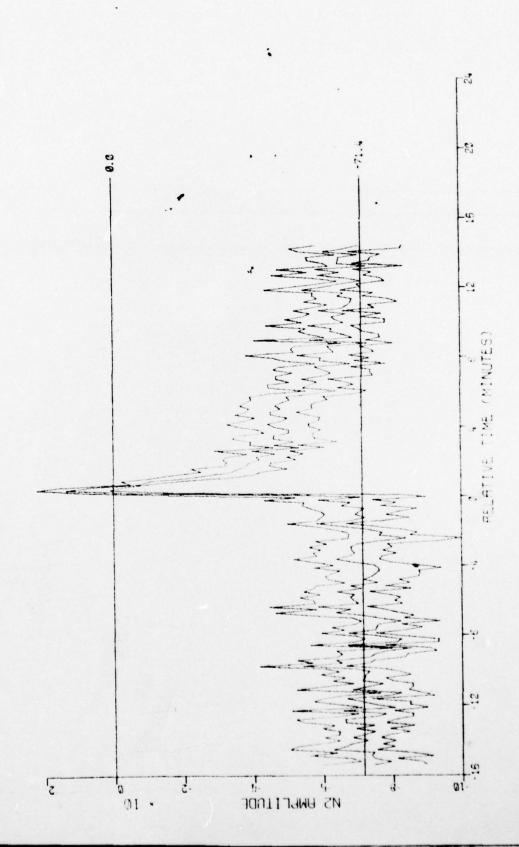


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ANIMAL A-0781 STIMULUS SITE 5. RECORDING SITE 1. EPOCH AVERAGED 10



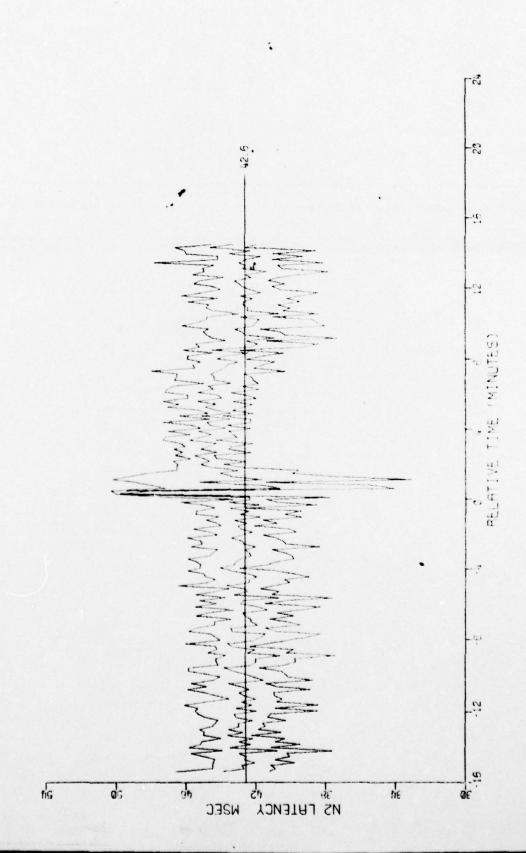
ACCELERATION 100.0 G RATE 4.67 /SEC NBR. AVERAGED 5 ANIMAL A:0761 STIMULUS SITE 5 RECORDING SITE EPOCH AVERAGED



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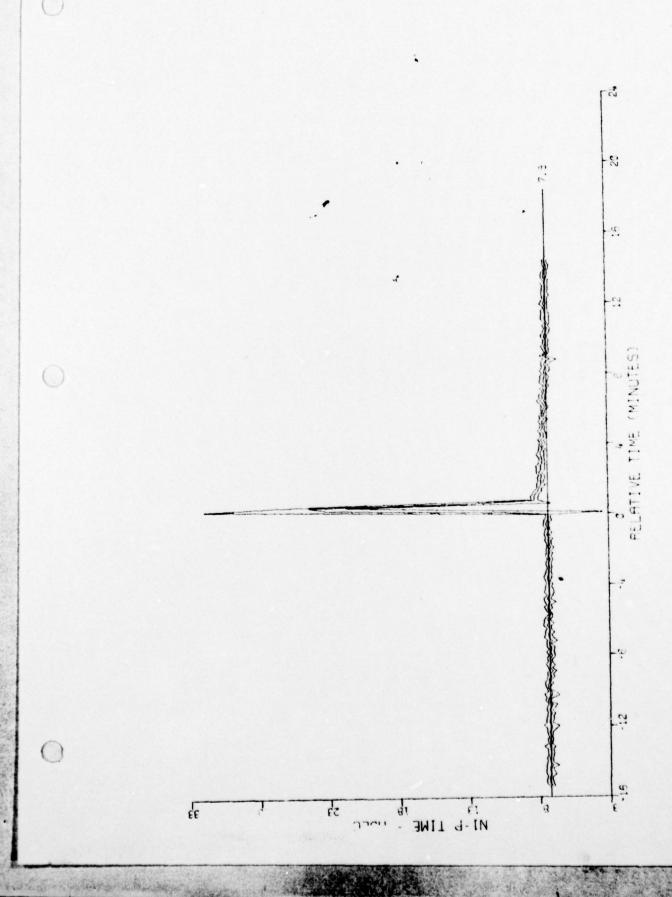
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ACCELERATION 100.0 G RATE 4.67 /SEC NBR. AVERAGED 5



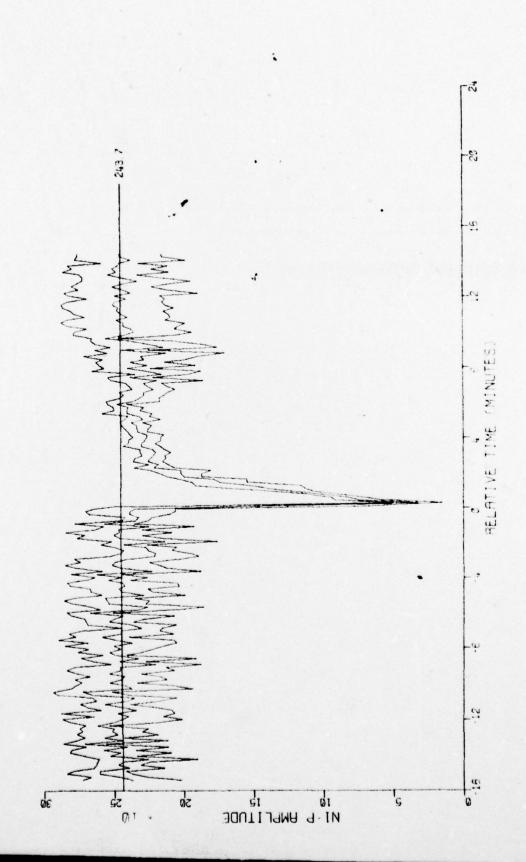
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ANIMAL A-0751
STIMULUS SITE 5. SPINE
RECORDING SITE 1. MX
EPOCH AVERAGED 10.26 SEC



AUN LX-3010 ANIMAL A-0761
STIMULUS SITE 5. SPINE
RECORDING SITE 1. MY
EPOCH AVERAGED 10.26 SEC

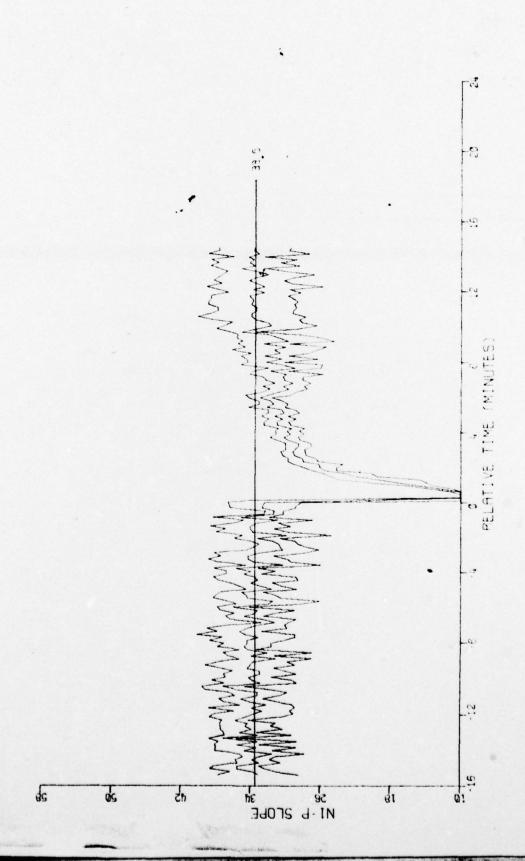
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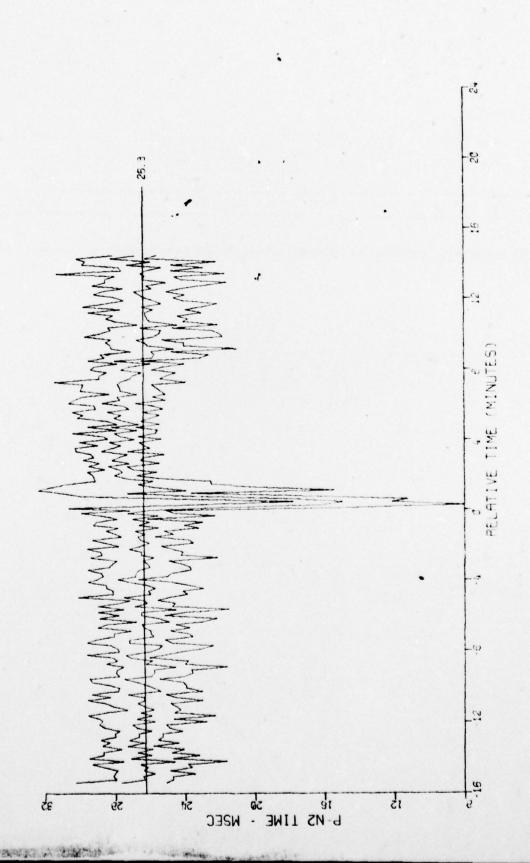
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RECORDING SITE 1. MX
EPOCH AVERAGED 10.26 SEC

ACCELERATION 100.0 G RATE 4.67 /SEC NBR. AVERAGED 5

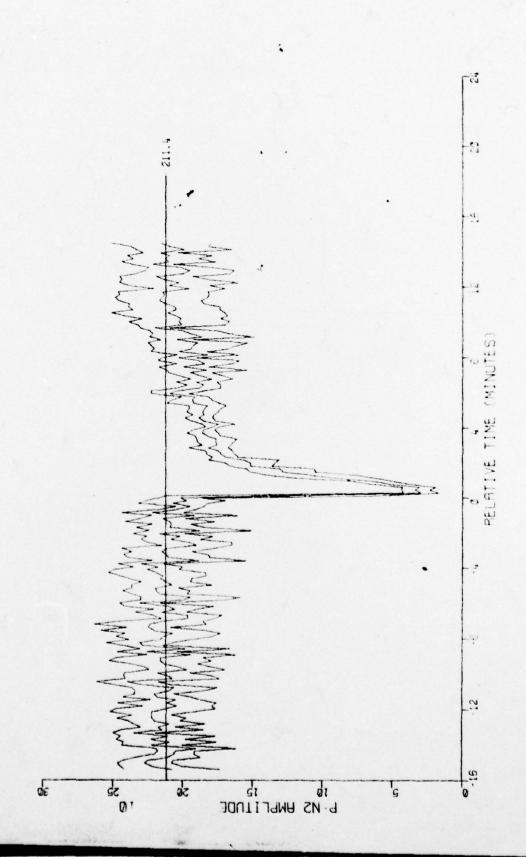


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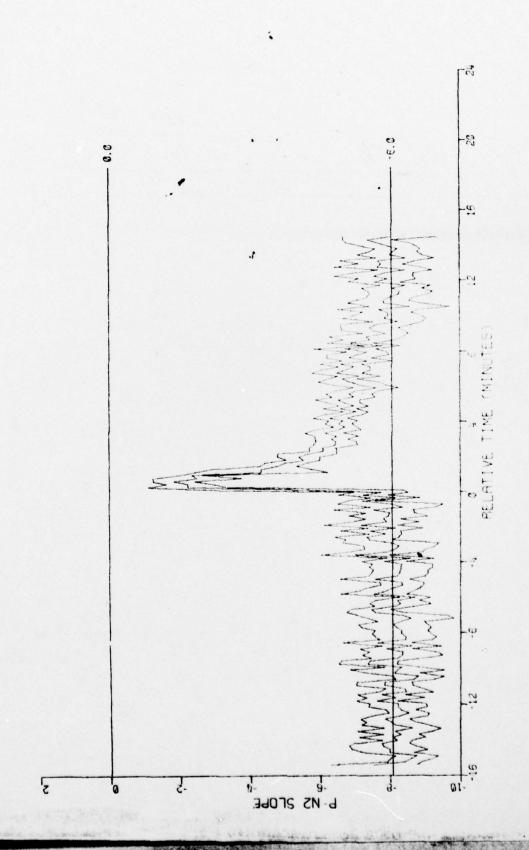
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ANIMAL A-0751
STIMULUS SITE 5. SPINE
RECORDING SITE 1. MX
EPOCH AVERAGED 10.26 SEC



ANIMAL A-0761 RUN STIMULUS SITE 5. SPINE RECORDING SITE 1. MX EPOCH AVERAGED 10.26 SEC

RATE 4.67 /SEC NBR. AVERAGED 5



ANIMAL A.0761
STIMULUS SITE 5. SPINE
RECORDING SITE 1. MX
EPOCH AVERAGED 10.26 SEC

ACCELERATION 100.0 G PATE 4.67 /SEC NBA, AVERAGED 5